

3D PRINTING

3D nanofabrication by volumetric deposition and controlled shrinkage of patterned scaffolds

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Lithographic nanofabrication is often limited to successive fabrication of two-dimensional (2D) layers. We present a strategy for the direct assembly of 3D nanomaterials consisting of metals, semiconductors, and biomolecules arranged in virtually any 3D geometry. We used hydrogels as scaffolds for volumetric deposition of materials at defined points in space. We then optically patterned these scaffolds in three dimensions, attached one or more functional materials, and then shrank and dehydrated them in a controlled way to achieve nanoscale feature sizes in a solid substrate. We demonstrate that our process, Implosion Fabrication (ImpFab), can directly write highly conductive, 3D silver nanostructures within an acrylic scaffold via volumetric silver deposition. Using ImpFab, we achieve resolutions in the tens of nanometers and complex, non-self-supporting 3D geometries of interest for optical metamaterials.

Most nanofabrication techniques currently rely on two-dimensional (2D) and 2.5D patterning strategies. Although popular direct laser writing methods allow for the single-step fabrication of self-supporting, polymeric 3D nanostructures (1–8), arbitrary 3D nanostructures (e.g., solid spheres of metal or metallic wires arranged in discontinuous patterns) are not possible (9, 10). This raises the question of whether a versatile 3D nanofabrication strategy can be developed that would allow independent control over the geometry, feature size, and chemical composition of the final material.

A hallmark of 2D nanofabrication strategies is that materials are deposited in a planar fashion onto a patterned surface. By analogy, we reasoned that a general 3D nanofabrication strategy could involve deposition of materials in a volumetric fashion into a patterned scaffold. However, such scaffolds face a fundamental tension:

They should be porous and solvated, to allow for introduction of reagents to their interior, while also being dense, to allow material placement with nanoscale precision. To resolve this contradiction, we reasoned that an ideal scaffold could be patterned in a solvated state and then collapsed and desiccated in a controlled way, densifying the patterned materials to obtain nanoscale feature sizes. Although several groups have experimented with shrinking materials, the shrinking process typically requires harsh conditions and chemical changes that may destroy functional materials (11–13). We use polyacrylate/polyacrylamide hydrogels for the scaffold material, as they have pore sizes in the range of 10 to 100 nm (14), they are known for their ability to expand and shrink up to ~10-fold in linear dimension (15–18), and methods for optically patterning hydrogels are well established (19–23).

Our implementation took place in three phases (24). It was previously found that two-photon excitation of fluorescein within acrylate hydrogels causes the fluorescein to react with the hydrogel (21–23). We took advantage of this phenomenon to attach fluorescein molecules carrying reactive groups to the expanded gel in defined 3D patterns (Fig. 1, A and B). In the second phase, after removal of the fluorescein patterning solution, the gel was functionalized by depositing materials onto the patterned reactive groups (Fig. 1, C and D) by using one of several available conjugation chemistries. This volumetric deposition step defines the composition of the material and may be followed by additional deposition chemistries (“intensification”) to boost the functionality of the deposited molecules or nanomaterials (Fig. 1, E and F). Importantly, the functional molecules or nanoparticles are not present during the patterning process, so the specific physical properties of the

molecules or nanoparticles used will not affect the patterning. In the final phase, the patterned and functionalized gel scaffold was shrunk by a factor of 10 to 20 in each dimension by using acid or divalent cations over a period of hours, and then it was dehydrated to achieve the desired nanoscale resolution (Fig. 1, G and H). The scaffold was not removed, as it supports the nanofabricated material and allows for the creation of disconnected or high-aspect-ratio structures that would otherwise collapse outside of the scaffold.

We found the polyacrylate gel to be a suitable substrate for patterning and deposition. The gel readily accommodated a wide variety of hydrophilic reagents, including small molecules, biomolecules, semiconductor nanoparticles, and metal nanoparticles (fig. S1, A to C). For laser powers below a critical threshold, the density of the deposited functional material was controllable (Fig. 1I and fig. S2). We estimated, based on the maximum pattern fluorescence (fig. S2A), that binding sites are patterned into the gel at concentrations of at least 79.2 μM in the expanded state, leading to a final concentration in the shrunken state of greater than 272.0 mM, or 1.64×10^{20} sites/ cm^3 for a 10 \times gel (see below). By repeating our patterning and deposition process, we were able to deposit multiple materials in different patterns in the same substrate, such as gold nanoparticles and cadmium telluride nanoparticles (Fig. 1J). We observed by using fluorescence that the deposition of the second material onto the first pattern was at most 18.5% of the deposition of the second material onto the second pattern, confirming that multiple materials may be independently patterned and deposited using this process (fig. S3).

The shrinking process is performed either by exposing the expanded gel to hydrochloric acid or to divalent cations (e.g., magnesium chloride) (fig. S1, A to C). The latter may be useful if the patterned materials are sensitive to acid, although we found that both streptavidin and DNA remained functionally intact after acid shrinking (fig. S1D). Gels that are shrunken in hydrochloric acid can subsequently be dehydrated, resulting in additional shrinking, and this process preserved the patterned geometry (Fig. 1K). The final dehydrated gel was transparent (fig. S4A), and atomic force microscopy (AFM) characterization measured the surface roughness over a 1- by 1- μm window to be ~0.19 nm (root mean square) (fig. S4B). Except where stated otherwise, all samples described as “shrunken” here were shrunken and dehydrated. We tested two different gel formulations that differed only in cross-linker concentration: 10 \times (0.075% cross-linker) and 20 \times (0.0172% cross-linker) (24). The 10 \times gels, and the patterns within, shrank consistently by a linear factor of 10.6 ± 0.8 in the lateral dimension (mean \pm SD, $n = 5$ gels) and 34.8 ± 1.8 in the axial dimension ($n = 6$ gels) (Fig. 1L), with the disproportionate axial shrink occurring during dehydration, possibly due to surface interactions between the shrinking polymer and the surface of the glass container. For the 20 \times gels, we observed 20.1 ± 2.9 -fold shrink

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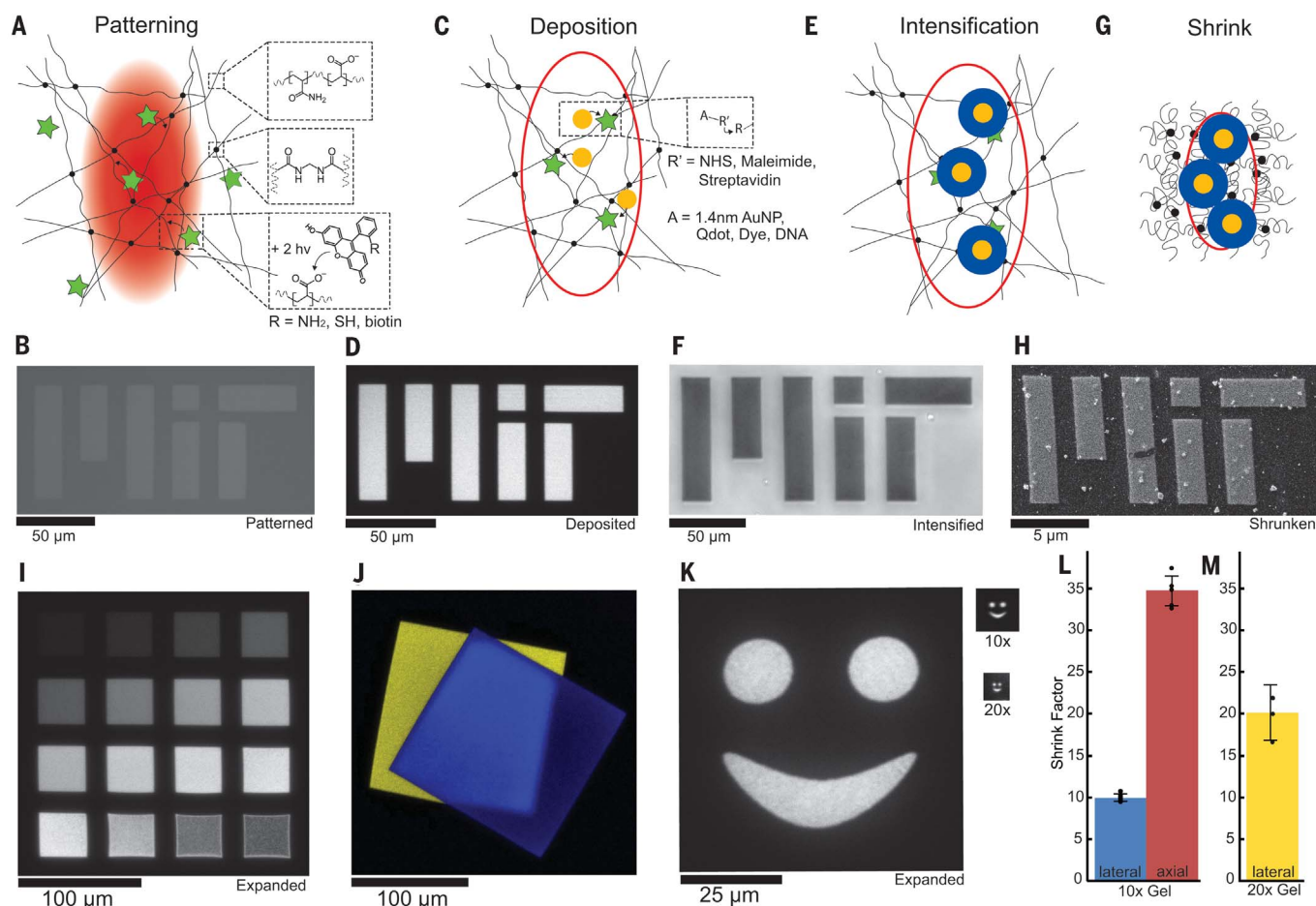


Fig. 1. The ImpFab process. (A) Schematic of the patterning process, showing the expanded polyelectrolyte gel (black lines and dots, top insets) and fluorescein (green star, bottom inset) binding covalently to the polymer matrix upon multiphoton excitation (red volume). Not to scale. Fluorescein bears a reactive group, R. h , Planck's constant; ν , frequency. (B) Residual fluorescence of patterned fluorescein immediately following patterning. (C) Schematic of functionalization of patterned gel by attaching small molecules, proteins, DNA, or nanoparticles to reactive R groups from (A). Red outline indicates patterned volume in (A). (D) Image of fluorescent streptavidin nanoparticle conjugates attached to the pattern in (B). (E) Schematic of the volumetric deposition process, showing growth of silver (blue) on top of gold nanoparticles within the

hydrogel matrix. (F) Image of silver deposited onto the pattern in (D) by transmission optical microscopy. Following silver growth, the pattern has high optical density. (G) Schematic of the shrinking and dehydration process. (H) SEM image of the silverized pattern from (F) following shrinking and dehydration. (I) Fluorescent patterns created with different laser powers (24). (J) Image of a gel patterned with both metal nanoparticles (yellow) and CdTe quantum dots (blue) in different locations. (K) Images of fluorescent patterns before shrinking (left, 10 \times gel), after shrinking and dehydration in a 10 \times gel (top right) and after shrinking and dehydration in a 20 \times gel (bottom right). (L) The mean lateral (blue) and axial (red) shrink factors (initial size/final size) for 10 \times gels ($n = 6$), including dehydration. (M) The mean lateral shrink factor for 20 \times gels (yellow; $n = 3$). Error bars show SD.

in the lateral dimension ($n = 4$ gels) (Fig. 1M). The 20 \times gel formulation is challenging to handle manually due to its delicacy, and so the axial shrink factor was not measured and they were not used further, except for distortion measurements.

To validate the minimum feature size of Implosion Fabrication (ImpFab), we designed a test pattern containing pairs of single-voxel-wide lines (Fig. 2, A to D). Because such postshrink features are necessarily below the optical diffraction limit, we deposited gold nanoparticles and employed scanning electron microscopy (SEM) to assess the resolution after shrinking. We estimated the resolution by measuring the line width [full width at half maximum (FWHM)] (Fig. 2, E to G) and obtained a value of 59.6 ± 3.8 nm

(mean \pm SD across samples, $n = 5$) (Fig. 2H) for 10 \times gels. The mean within-sample standard deviation of the line width was 8.3 nm. We estimated the isotropy of the shrinking process by calculating the ratio of the longest diameter of the patterned circle to the orthogonal diameter (Fig. 2, C and D). The percent distortion thus calculated was $6.8 \pm 6.9\%$ for 10 \times gels (mean \pm SD, $n = 6$ gels) and $8.2 \pm 4.3\%$ for 20 \times gels ($n = 4$ gels). We found that the ratio of axial to lateral shrink was on average within $3.1 \pm 2.5\%$ of the mean of this ratio ($n = 6$ 10 \times gels), indicating that the disproportionate axial shrink is highly reproducible. Thus, it is possible to account for the disproportionate axial shrink in the design of the pattern. To illustrate this point with the fabrication of a cube, we patterned a rectangular prism

and imaged it before and after dehydration (fig. S5). As expected, the rectangular prism contracted in the axial dimension during the dehydration step and turned into a cube.

Because nanoscale metal structures are broadly important in fields such as nanophotonics, metamaterials, and plasmonics, we applied ImpFab to create conductive silver structures. We anchored gold nanoparticles to patterned amines via a biotin-streptavidin linkage (24). We were initially unable to deposit gold nanoparticles at high enough concentrations to form conductive structures. We thus developed an intensification process based on photographic intensification chemistries, in which silver was deposited onto the surface of gel-anchored gold nanoparticles in aqueous phase while the gel was in the expanded

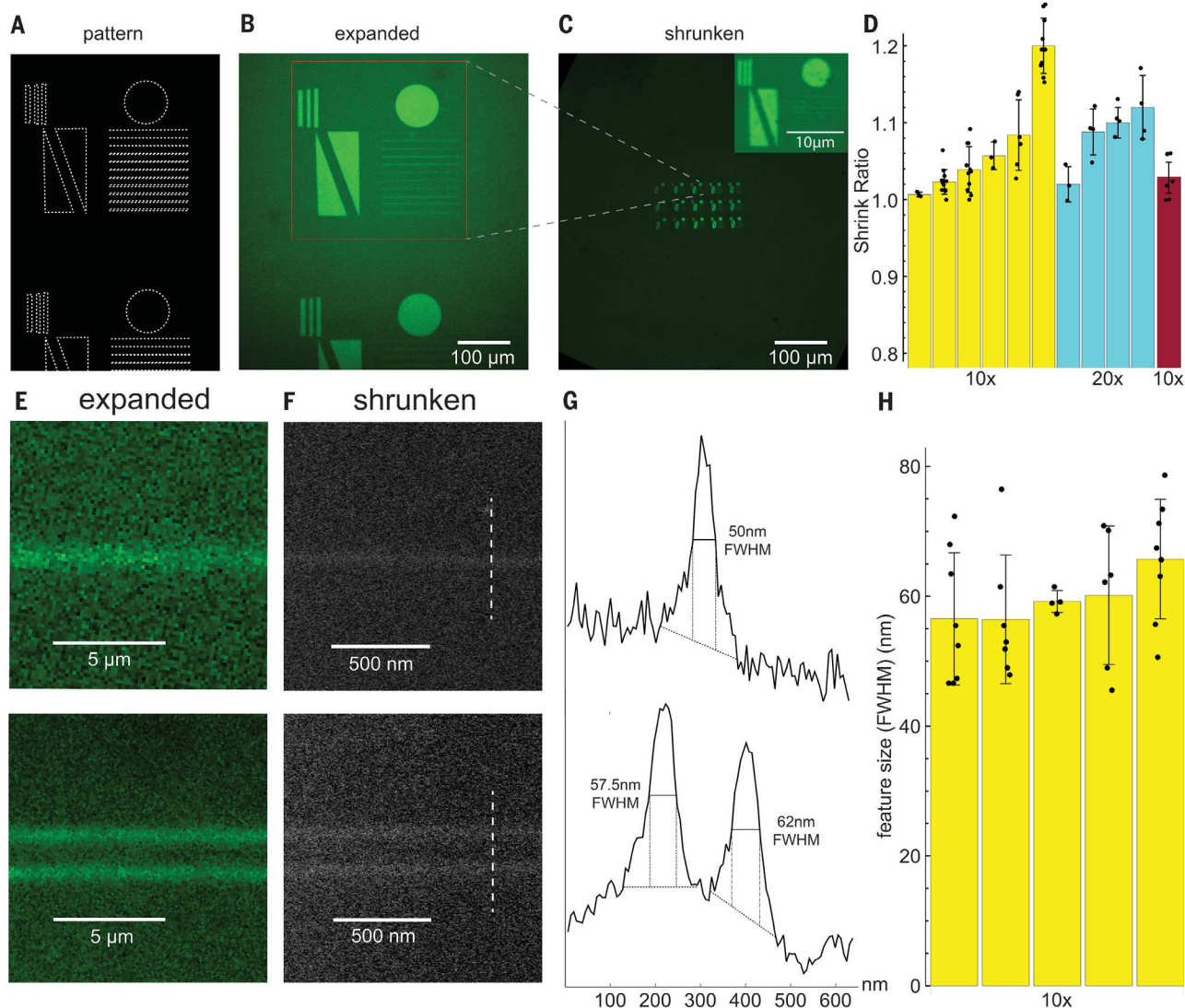


Fig. 2. Resolution of implosion fabrication. (A) Design of the resolution test pattern, including pairs of single-voxel-thick lines (bottom right). (B) Fluorescence image of the patterns from (A). (C) Fluorescence image of the pattern from (B) after shrinking. (D) Measures of isotropy in lateral and axial dimensions. Yellow and blue bars represent lateral isotropy for 10× gels and 20× gels, respectively, and the red bar represents axial isotropy for 10× gels. (E) Fluorescence images of single-voxel lines before

shrinking. (F) SEM images of single-voxel lines after 10× shrinking. The gel was functionalized with gold nanoparticles for contrast. (G) Cross-sectional intensity profiles of the lines imaged by SEM [dashed lines in (F)], showing how the FWHM of single voxel lines were measured. (H) Line widths, measured in (G), for five different gel samples. Dots are measurements for individual lines; bars indicate means \pm SD, across individual lines within a single gel.

state (Fig. 1, E and F). Finally, the gel was treated with a chelating agent to remove any remaining dissolved silver and was then shrunk via exposure to hydrochloric acid and subsequent dehydration.

Even with the silver intensification process, wire structures fabricated using the method above (Fig. 3A) were not reliably conductive, or they had resistances on the order of hundreds of ohms. We tested several different methods of sintering, including treatment with oxygen plasma, electrical discharge, and heating the sample to $\sim 500^\circ\text{C}$ in an oven. However, none of these methods resulted in well-preserved and evenly sintered silver structures. Instead, we found that the silver patterns could be sintered effectively

when we used the same two-photon setup used for the initial photopatterning step. We found that samples irradiated at relatively low power levels (24) showed a distinct change in the morphology of the embedded silver nanoparticles that was consistent with sintering (Fig. 3, B and C). We measured the conductivity of three patterned silver squares both before and after sintering and found that the resistance of each square decreased by 20- to 200-fold (Fig. 3D). Sintered wires were measured in a four-point probe system and were found to have linear IV curves (fig. S6A). Wires sintered in this way had an average resistance of 2.85 ± 1.68 ohms (mean \pm SD, $n = 10$), with the resistance depending on the density of the patterned silver

(fig. S6B). By contrast, an ideal silver wire with the same geometry would have a resistance of 0.38 ohms, suggesting that our sintered structures achieved a mean conductivity 13.3% that of bulk silver, with individual samples obtaining conductivities as high as 30% that of bulk silver (Fig. 3E).

To verify that our method is compatible with a wide range of 3D geometries, we fabricated structures with dimensions ranging from hundreds of nanometers to several micrometers (Fig. 4, A to C). We found that these structures retained their morphology following sintering (Fig. 4B). We fabricated a nonlayered, nonconnected 3D structure comprised of many 2D substructures arranged at different angles relative to each other

in space, which would not lend itself to fabrication by other means (Fig. 4D). Whereas our previous experiments had only observed the fabrication of 2D silver structures, we used confocal reflection microscopy to confirm that

silver was deposited throughout the volume of the 3D pattern (Fig. 4E). Finally, using confocal microscopy, we were able to validate that the structure retained its shape after shrinking (Fig. 4F).

Due to the modular nature of ImpFab, the extension of the ImpFab strategy to other kinds of materials, such as other semiconductors or metals, only requires the development of an aqueous deposition chemistry that is compatible

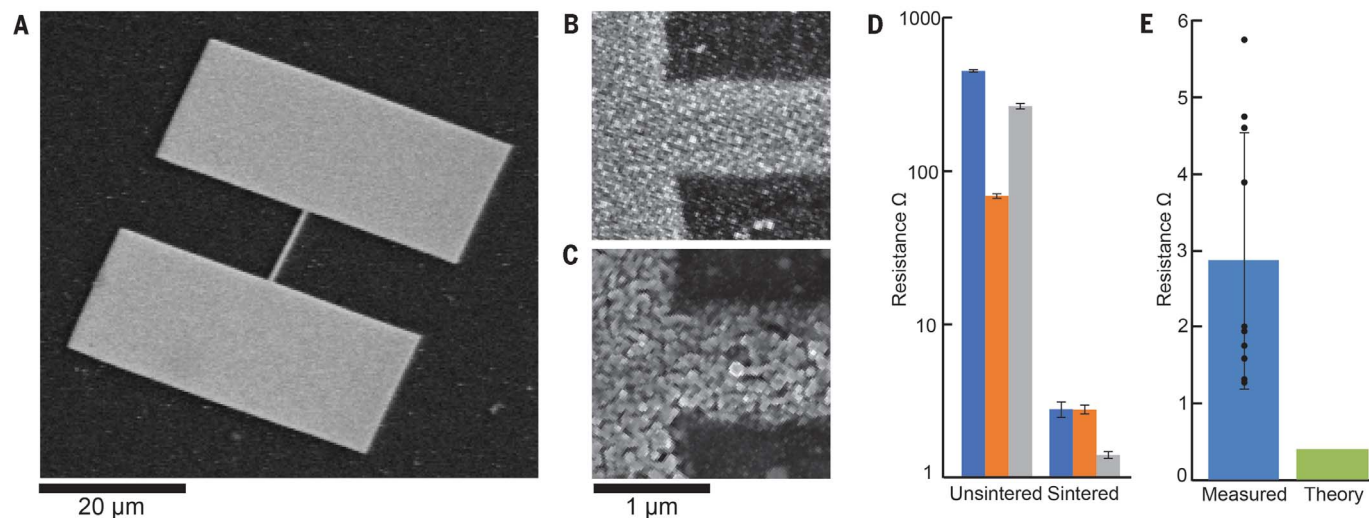
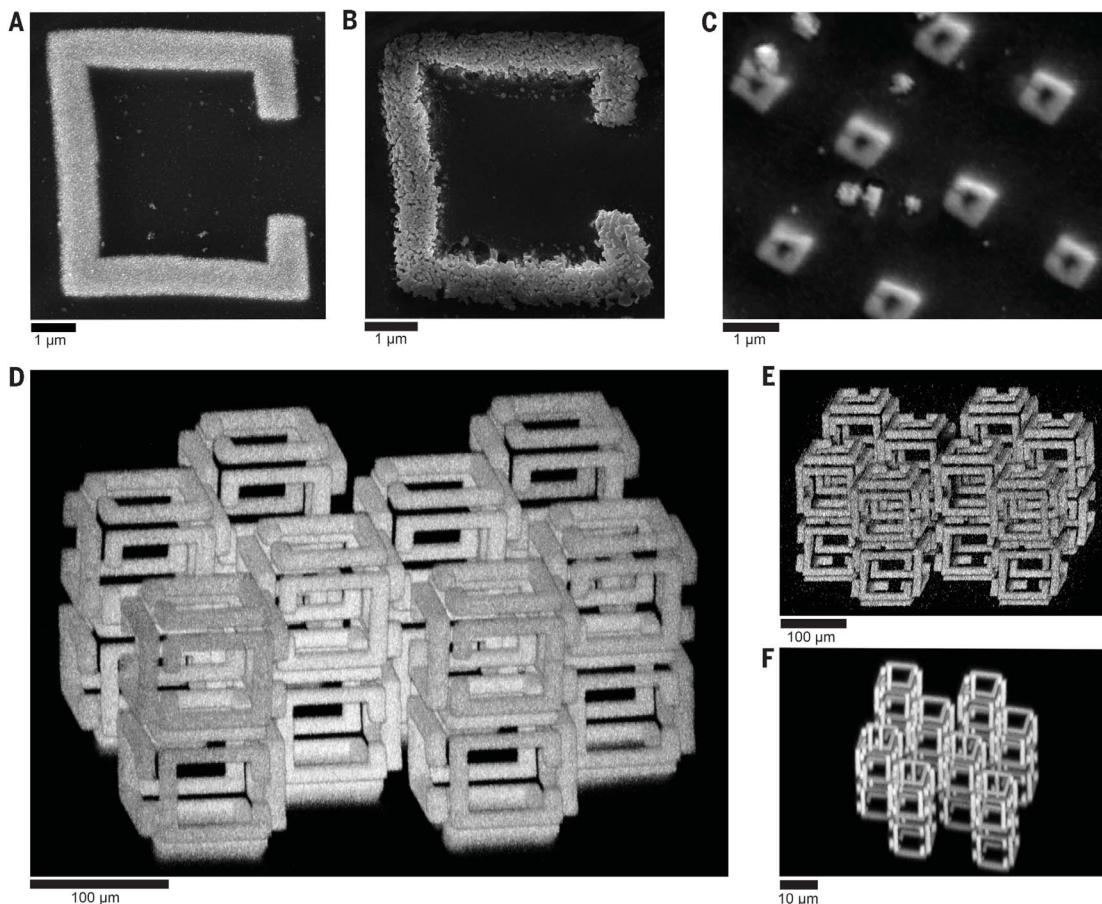


Fig. 3. Characterization of silver conductivity. (A) SEM overview of a shrunken silver wire between two landing pads, prior to sintering. (B and C) SEM images of wires before (B) and after (C) sintering. (D) Resistance of three separate conductive pads, each with dimensions of 35 μm by 35 μm , measured before and after sintering. Each color represents

a single conductive pad. Error bars show standard errors in a four-point conductivity measurement. (E) Resistance of individual sintered wires (black dots) and the means (blue) and standard deviations, compared to the theoretical conductivity of a similar structure made of bulk silver (green).

Fig. 4. Fabrication of 3D metal nanostructures.

(A and B) 2D structures fabricated with ImpFab with micrometer-scale resolution, before (A) and after (B) sintering (visualized via SEM). (C) Similar structures fabricated with a 100-nm feature size, after shrinking and dehydration but before sintering. (D) Maximum-intensity projection of a fluorescent image of a 3D structure before shrinking (2, 28). (E) Maximum-intensity projection of a reflected light image from the same structure following volumetric silver deposition, prior to shrinking. (F) Maximum-intensity projection of a fluorescent image of the same structure shrunken but not dehydrated.



with the gel substrate. Future iterations may use alternative chemistries, such as dendrimeric complexes for direct deposition of metals or semiconductors within the hydrogel (25, 26), or DNA-addressed material deposition (27). Finally, we note that although we used a conventional microscope that was not optimized for patterning and that was limited to a 4-cm/s scan speed (in postshrink dimensions), we were able to create objects spanning hundreds of microns to millimeters (fig. S7). With the use of faster patterning systems (23), ImpFab could ultimately enable the creation of centimeter-scale nanomaterials.

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SUPPLEMENTARY MATERIALS

www.sciencemag.org/content/362/6420/1281/suppl/DC1
Materials and Methods
Figs. S1 to S7
Tables S1 to S3
Data S1

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Shrinking problems in 3D printing

Although a range of materials can now be fabricated using additive manufacturing techniques, these usually involve assembly of a series of stacked layers, which restricts three-dimensional (3D) geometry. Oran *et al.* developed a method to print a range of materials, including metals and semiconductors, inside a gel scaffold (see the Perspective by Long and Williams). When the hydrogels were dehydrated, they shrunk 10-fold, which pushed the feature sizes down to the nanoscale.

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