BioEngineering 221/Radiology 221

Production of Radionuclides & Interaction of Radiation with Matter

January 16, 2018

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Aspects of the Radiotracer

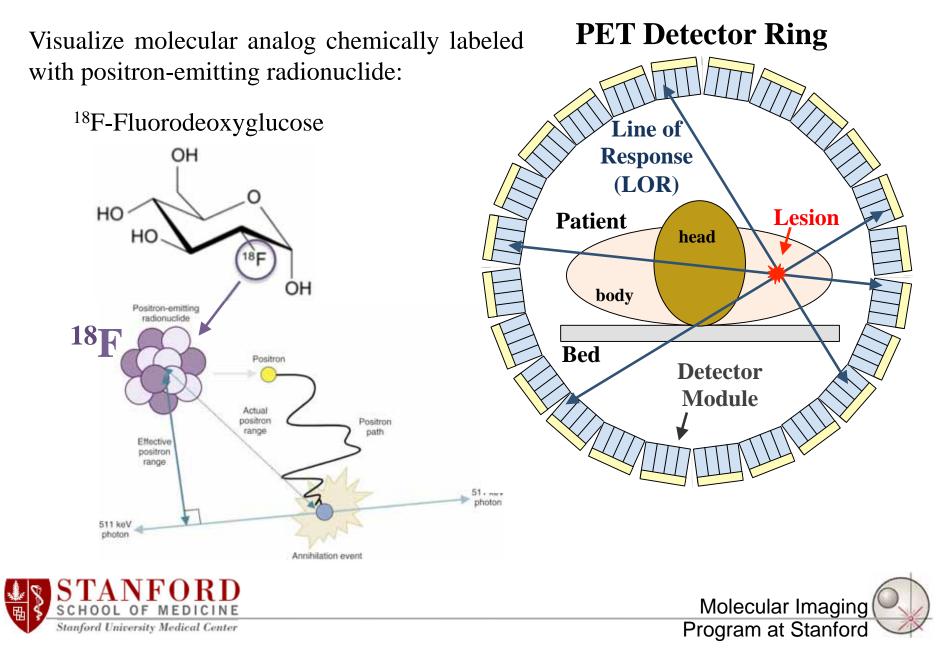


- What modes of radioactive decay are used?
- How do radionuclides decay to produce emissions for imaging?
- How are relevant radionuclides produced?
- How do radionuclide emissions interact in tissue and detectors?





Illustration of Course thus Far and Future

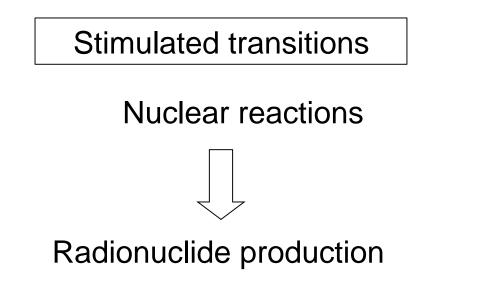


Production of Radionuclides





Nuclear transitions & Radioactive Decay



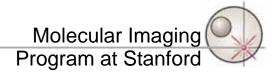
Spontaneous transitions

- α decay
- β decay
- γ de-excitation

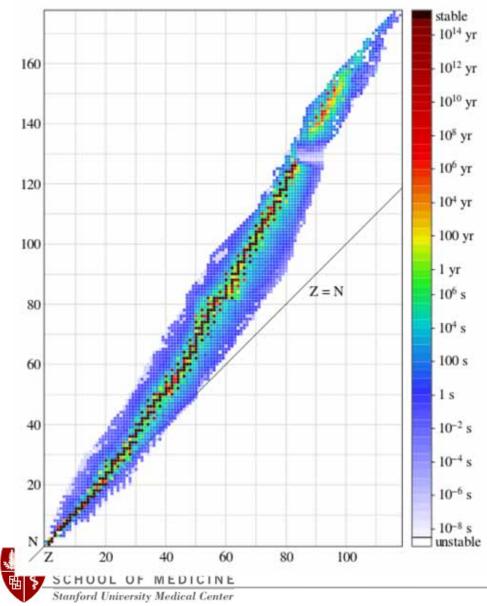
Increase Energy

Decrease Energy



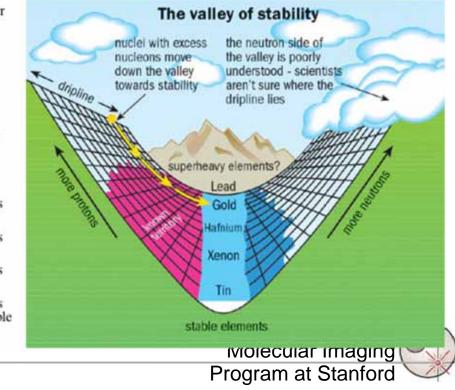


Nuclear Transitions



 Adding energy to the nuclei, pushes nuclei to the edge of the valley of stability
 Energy peeded for this

• Energy needed for this process



Producing Radioactive Nuclei

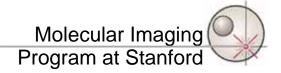
- Naturally occurring radioactive isotopes :
 - Typically have long half-life
 - Very heavy elements that are not endogenous to human biology



Use methods to produce radioactive isotopes

Produced through **Nuclear Reactions**





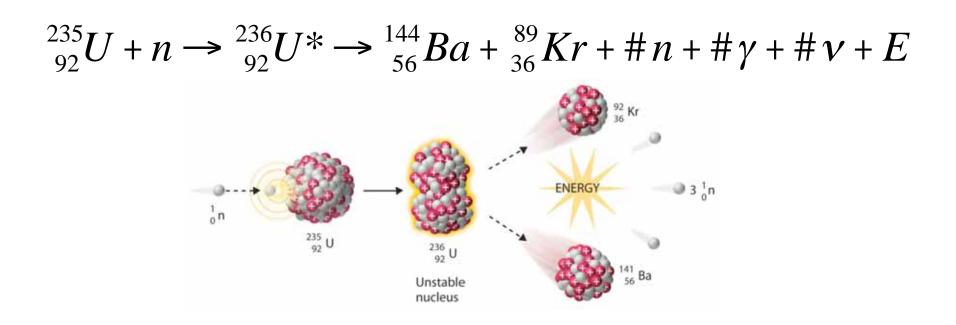
Overview

- **1. Reactor-Produced** Radionuclides: Neutron activation and fission products
- **2. Accelerator-Produced** Radionuclides: Proton activation and cyclotron
- 3. Radionuclide **Generators** (^{99m}Tc)





A common neutron source



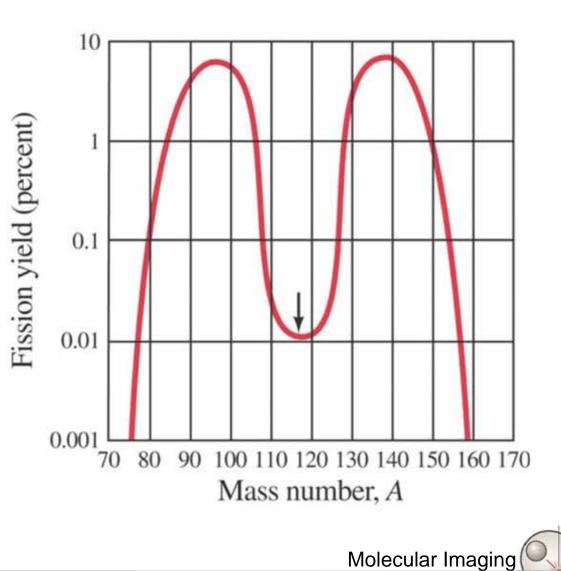
- Stimulated fission is the **source of energy** in a nuclear power plant
- Production of a statistical # of neutrons enables a **chain reaction**
- Excited ²³⁶U has more than 100 nuclides among its fission products





Fission Yield of U-235

- In general one fragment with A between 130 and 150; and another between 85 and 105
- Fission products with equal masses are least likely

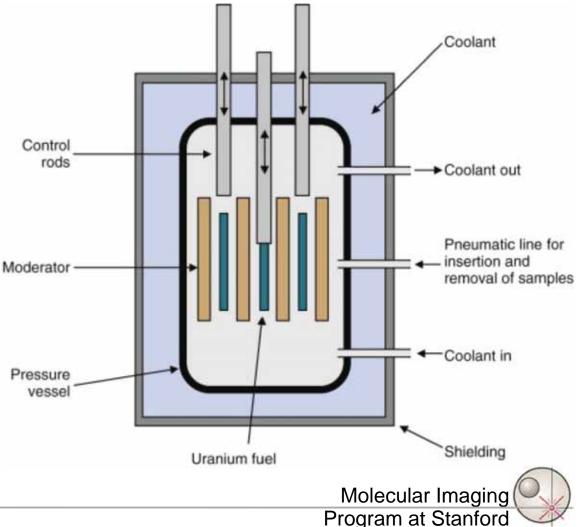


Program at Stanford



A Nuclear Reactor

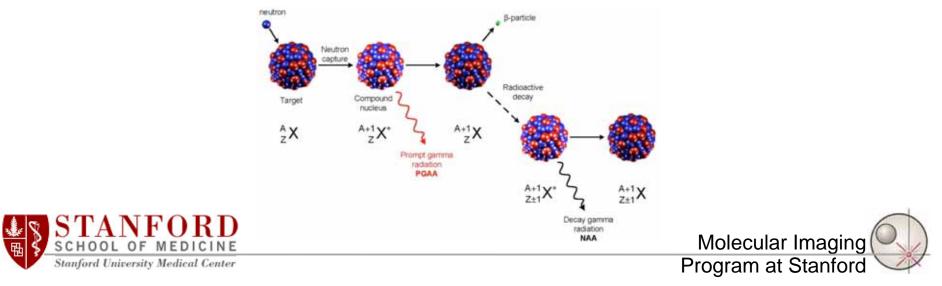
- Nuclear reactors have provided large quantities of radioactive isotopes for nuclear medicine
- Fuel cells contain fissionable material (~4-5% of U-235 by weight)
- Moderator to slow down the neutrons (water or 'heavy' water D₂0)
- Control rods contain strong neutron absorbers to moderate the reaction
- Each fission events creates about ~200 MeV of energy, mainly released as heat to moderator
- Radionuclides are produced in samples surrounding the reactor core



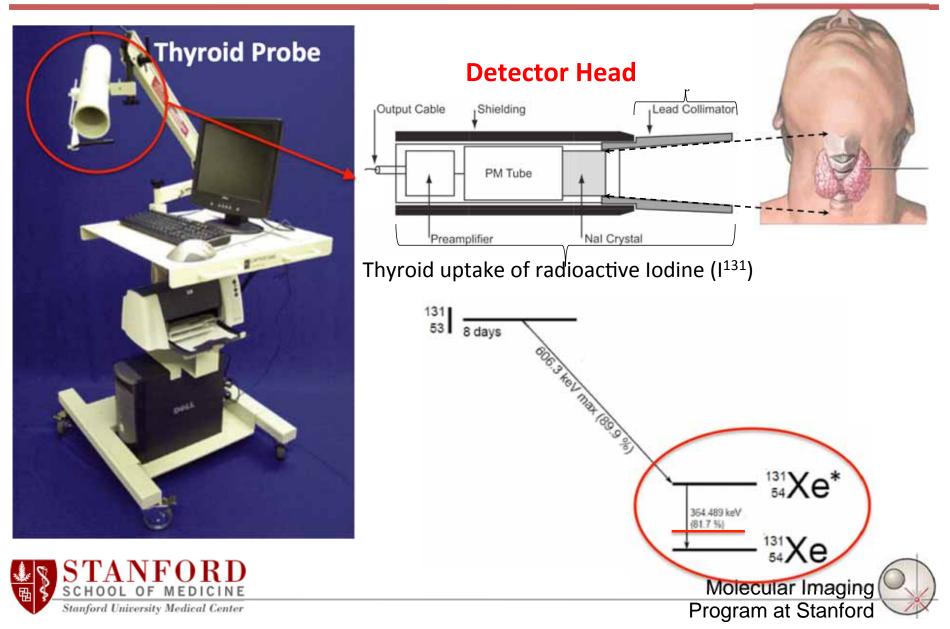


Reactor produced Radionuclides

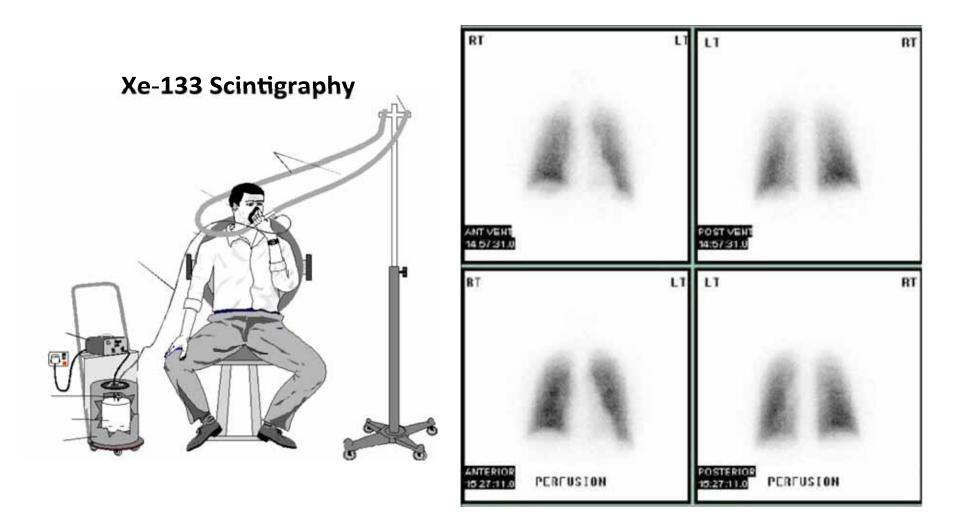
- Fission products have excess neutrons and thus decay by $\beta^{\text{-}}$ decay
- If a radioactive intermediate has sufficiently long half-life it can be extracted and used as a medical radionuclide ${}^{99}_{39}Y \xrightarrow{\beta^-,1.5s} {}^{99}_{40}Zr \xrightarrow{\beta^-,21s} {}^{99}_{41}Nb \xrightarrow{\beta^-,15s} {}^{99}_{42}Mo(T_{1/2} = 65.9hr)$
- ⁹⁹Mo is used to generate ^{99m}Tc (More on this in just a bit)
- Also ¹³¹I and ¹³³Xe produced by neutron activation, these are important for nuclear medicine as well



Reactor produced Radionuclides



Reactor produced Radionuclides



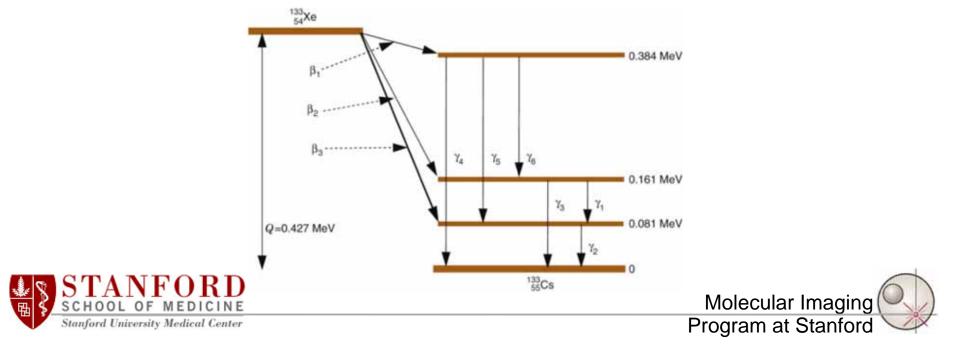


Molecular Imaging Program at Stanford

Radionuclides by fission

General properties:

- Excess of neutrons, hence β^- decay
- Products may be carrier free, thus radionuclides have high specific activity by chemical separation
- Lack of specificity in fission products is a drawback



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Nuclear reactions: proton activation

Proton needs to be energetic to make it to the atomic nucleus, typically 10-20 MeV

- → Need particle accelerators
- Different kind of particle accelerators
- Most common: cyclotron

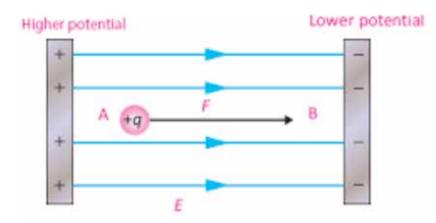




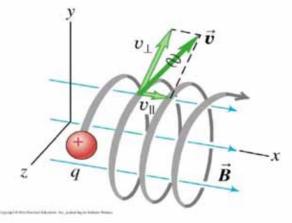
Proton acceleration: Cyclotron

- Charged particle in electric field: acceleration
- Charged particle in magnetic field: change of direction

→ These principles are combined in a cyclotron.



Motion of charged particles in a magnetic field





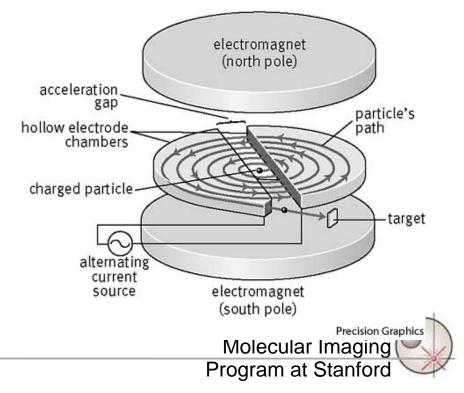


Proton acceleration: Cyclotron

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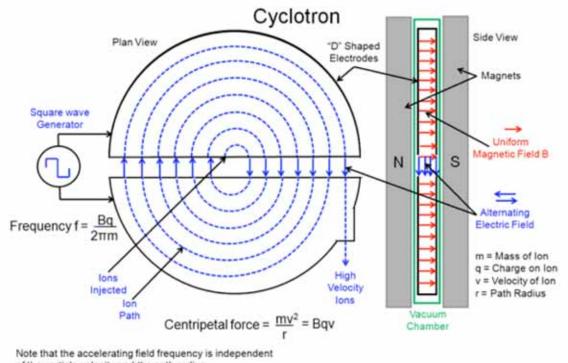
→ These principles are combined in a cyclotron.

- Pair of hollow 'dees', positioned between poles of magnet
- Ion source at the center
- Electric field between dees





Proton acceleration: Cyclotron



- of the particle velocity and the path radius
- Particle gains energy in gap between dees
- Upon increased energy, the ion will have a larger radius in the dee
- Electric field is reversed after every transition



Molecular Imaging Program at Stanford

Proton acceleration: cyclotron

- When maximum orbital radius is reached, particles are extracted, using targets or a stripping foil
- Cyclotron produce in general smaller quantities of radioactivity than nuclear reactors due to
 - Lower beam intensities
 - Lower cross section
- Special interest are short-lived positron emitters: ¹¹C (20 min), ¹³N (10 min), ¹⁵O (2 min), these require a local cyclotron
- Also ¹⁸F (110 min) important, but a regional distribution center is sufficient





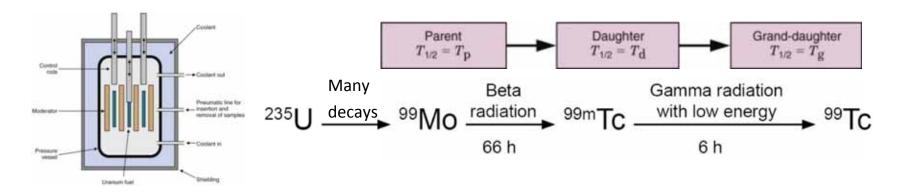
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Radionuclide Generators

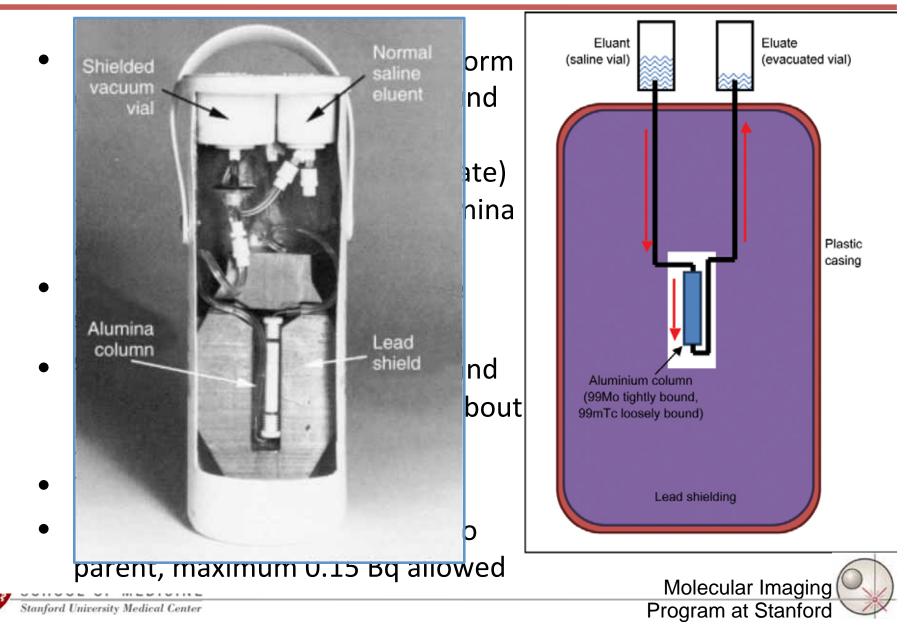


- Parent-daughter radionuclide pair contained in apparatus that permits separation
- Most important generator: ⁹⁹Mo ^{99m}Tc
- Very common because of wide spread Tc use (more than 1850 TBq of ⁹⁹Mo required *per week*)
- Also ⁶⁸Ga, ⁸²Rb, ⁶²Cu are generator produced





Radionuclide Generators



Radiotracers

- Many candidate radionuclides, yet relatively small number of practical radionuclides because of following considerations:
 - Type and energy of emissions and the branching ratio: ideally no other processes than γ-emission at energies 50-600 keV
 - Physical half-life of radionuclide:
 - If too short: no time for preparation
 - If too long: high radiation contamination for disposal and most of the activity emitted outside of examination time
 - **Specific activity**: need as many as possible radioactive molecules in a sample; must not be biologically perterbing
 - **Radionuclidic purity:** fraction of the radioactivity in the desired form, i.e. no contaminants
 - **Cost and complexity:** ease of production





Radiotracers

Radionuclide	Decay Mode	Principal Photon Emissions	Half-Life	Primary Use
¹¹ C	β+	511 keV	20.4 min	Imaging
¹³ N	β+	511 keV	9.97 min	Imaging
¹⁵ O	β+	511 keV	2.03 min	Imaging
¹⁸ F	β+	511 keV	110 min	Imaging
³² P	β–	—	14.3 d	Therapy
⁶⁷ Ga	EC	93, 185, 300 keV	3.26 d	Imaging
⁸² Rb	β+	511 keV	1.25 min	Imaging
⁸⁹ Sr	β—	—	50.5 d	Therapy
^{99m} Tc	IT	140 keV	6.02 hr	Imaging
¹¹¹ In	EC	172, 247 keV	2.83 d	Imaging
¹²³	EC	159 keV	13.2 hr	Imaging
125	EC	27-30 keV x rays	60.1 d	In vitro assays
¹³¹	β—	364 keV	8.04 d	Therapy/imaging
¹⁵³ Sm	β—	41, 103 keV	46.7 hr	Therapy
¹⁸⁶ Re	β—	137 keV	3.8 d	Therapy
²⁰¹ TI	EC	68-80 keV x rays	3.04 d	Imaging





Production of Radionuclides: Major Takeaways

- 1. Naturally abundant radionuclides are long-lived, not generally useful for nuclear medicine studies
- Produce short-lived radionuclides via stimulated transitions: ex. neutron activation or fission in reactor, proton activation in cyclotron
- 3. Work horse isotope Tc-99m eluted from Mo-99 product in radionuclide generator
- Radionuclide chemically labeled to biological analog, which predetermines application, specificity, and so much





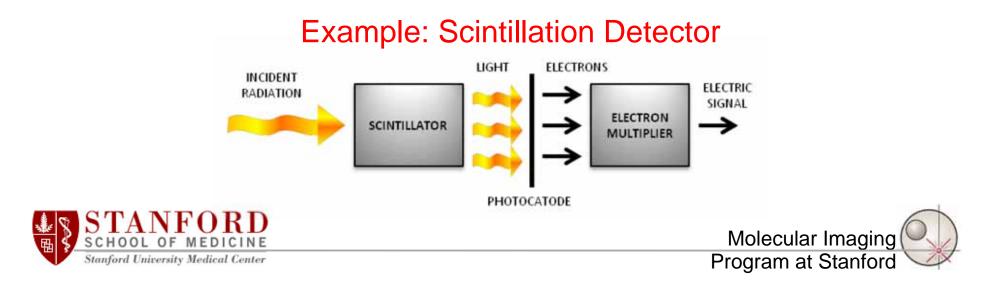
Interaction of Radiation with Matter



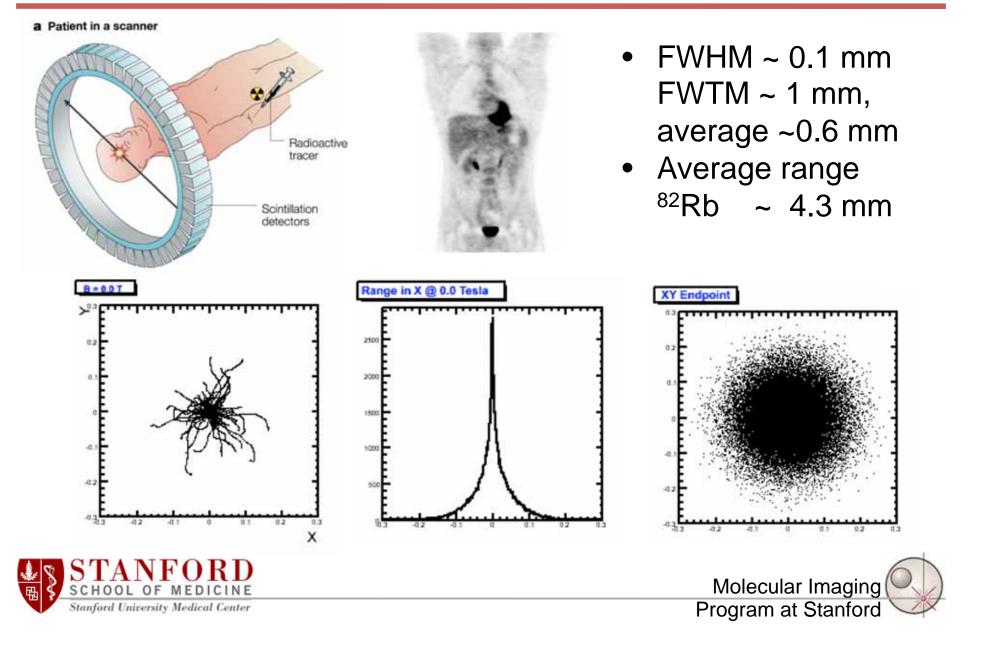


Interactions of rad. with matter: How it fits in

- Why is understanding interaction of radiation with matter important for imaging in nuclear medicine?
- Emissions from radioactive nuclei are too high in energy & too small to be seen with the naked eye
- We observe their existence only through the effects they produce in matter
- Effects caused by various forces and interactions the nuclear emissions experience as they traverse a material

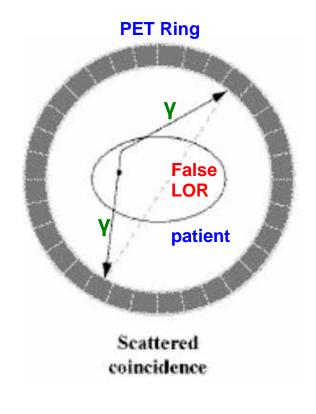


Range of ¹⁸F positrons in water



Interactions of rad. with matter: How it fits in

- The forces and interactions that nuclear emissions experience can also alter the state of the emissions
- This can directly impact imaging, ex. Compton scatter in PET:







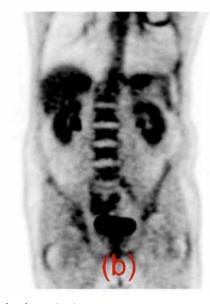
Interactions of rad. with matter: How it fits in

• The forces and interactions that nuclear emissions experience can also alter the state of the emissions

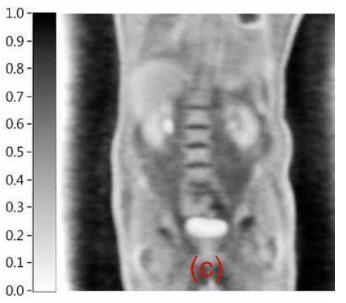
(a) Scatter Correction



(b) No Scatter Correction



Difference (b)-(a)/(b)

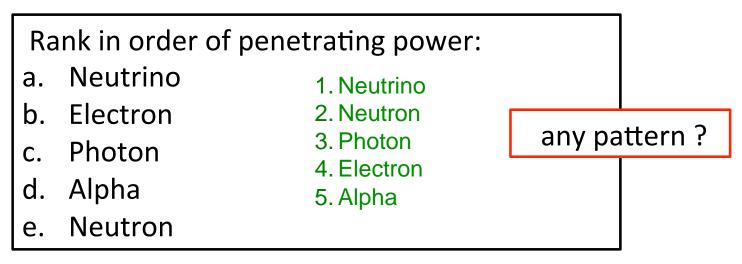






Intro: interaction of radiation with matter

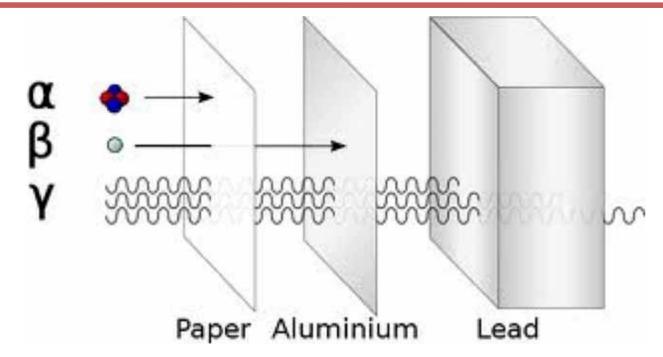
• Examples of highly penetrating radiation ?







Intro: interaction of radiation with matter



• Incoming radiation interacts with the *electrons or the nucleus* of the material it encounters

Tissue penetration dependent on:

- 1. Type of Radiation
- 2. Interaction Material (and thickness)





Intro: interaction of radiation with matter

- Important for *detection* of radiation, assessing *radiation damage*, analyzing *radiation therapy*
- density p and atomic number Z of the interacting matter is important
- Interactions are statistical in nature:

$$P_{\rm int} = 1 - e^{-\mu x}$$

- μ = attenuation coefficient (1/cm)
- x = distance travelled
- 1/µ = *mean* free path
- Many particles per unit length so low variations in average numbers





Interaction of radiation with matter

Distinction between three types:

1. Heavy charged particles:

- Short, well defined range
- Collisional losses (at Nuc Med energies)

2. Light charged particles:

- Longer, largely varying paths
- Collisional and some radiative losses
- 3. Photons
 - Rayleigh Scatter (non-ionizing)
 - Photo-electric Effect
 - Compton Scatter
 - Pair Production

Interaction of Ionizing radiations will ultimately result in a cascade of lower energy electrons



Molecular Imaging Program at Stanford

Intro: interaction of radiation with matter

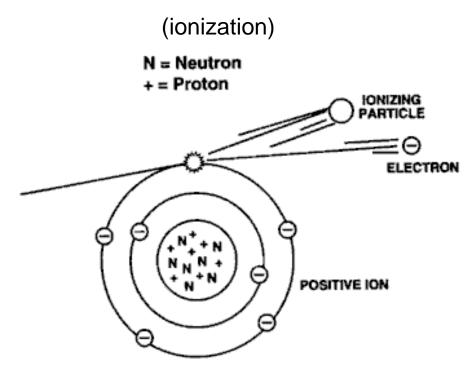
- Charged particles undergo two primary energy transfer mechanisms:
 - Collisional Energy Transfers
 - Radiative Energy Transfers





I: Collisional losses

Collisional losses



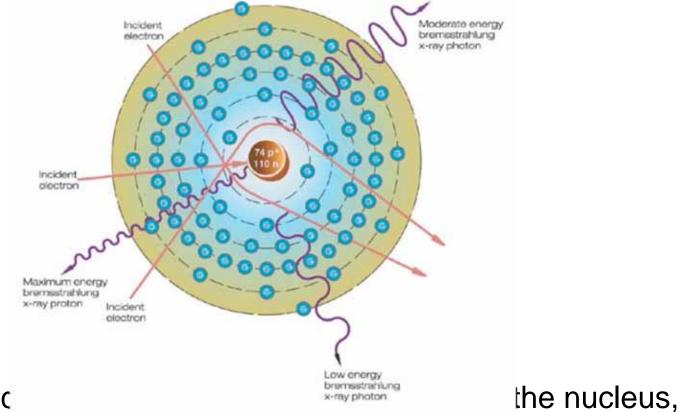
- When incoming radiation has a lot of kinetic energy, it may ionize the material; i.e. we have **ionizing radiation**
- Alternative: excitation of the atom (elastic)



Molecular Imaging

II: Radiative losses

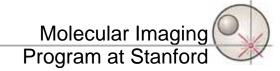
Competing process: Radiative loss



Charged partic

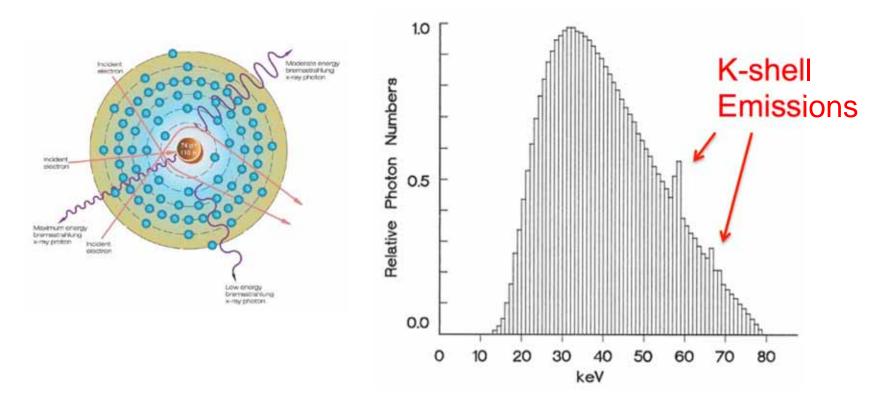
loses energy, emits a Bremsstrahlung photon





II: Bremsstrahlung

Results in a continuum of energies produced:





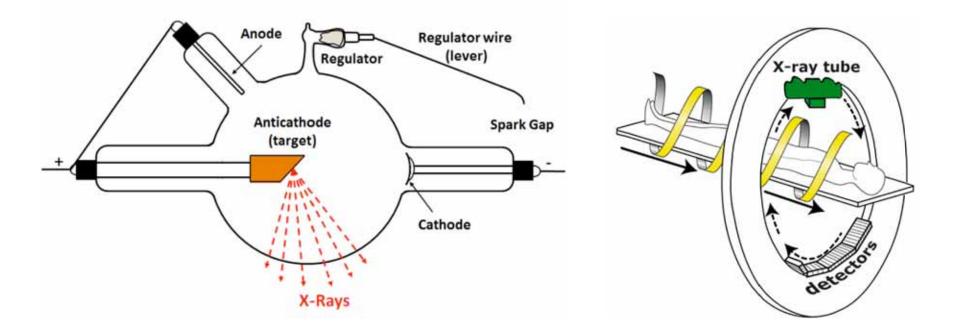
Molecular Imaging

II: Bremsstrahlung

Xray-CT Imaging exploits bremsstrahlung to visualize anatomy

X-ray tube

X-ray CT Scan







I: Heavy Charged Particles

- Interact mainly through Coulomb interaction with atomic electrons
- Range is short: 10 MeV proton loses all its energy in only 0.25 mm copper
- Inelastic scattering: # particles in ≠ # particles out:
 α + Z → α + Z⁺ + e⁻
- Energy transferred to the atom
- Ionizing radiation: target becomes ionized, may yield biological damage
- Other interaction may be elastic scattering from nucleus, or nuclear reactions





II: Light Charged Particles: Electrons/Positrons

- Electrons behave similarly as heavy charged particles
- Lose energy through interactions with atomic electrons, *however* :
 - More energy is transferred in a collision
 - Secondary electrons may become ionizing: *delta-rays*
 - Path subject to large variations
- Q: What about positrons ?
 - A: exactly the same, except for *annihilation* after thermalization



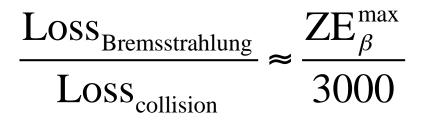


Bremsstrahlung vs Collisional Losses

- Okay so there are two competing processes: Collisional and radiative energy transfers
- Which is dominant?
- Relatively more Bremsstrahlung at higher or lower energies ?
- Relatively more Bremsstrahlung at high Z or low Z?

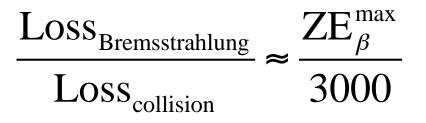






- Radiative losses more prominent for increasing particle energy and increasing absorber Z
- Radiative losses more prominent for increasing particle energy

Are radiative (bremsstrahlung) or collisional losses more dominant for charged particles at energies relevant to nuclear medicine imaging studies?



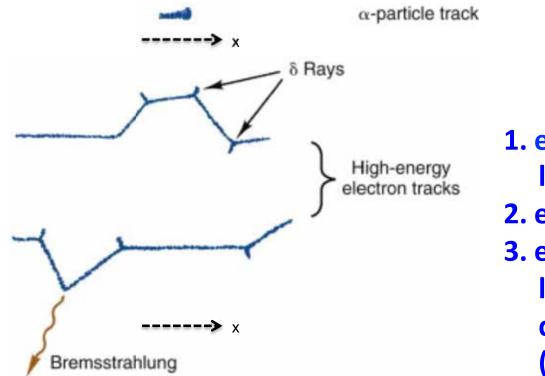
Are radiative (bremsstrahlung) or collisional losses more dominant for charged particles at energies relevant to nuclear medicine imaging studies?

$$\frac{\text{Loss}_{\text{Bremsstrahlung}}}{\text{Loss}_{\text{collision}}} \approx \frac{\text{ZE}_{\beta}^{\text{max}}}{3000}$$

- Z for tissue is low H20 ~7.4
- Energy range for nuclear medicine studies ~0.1-0.5 MeV

Very small fraction of energy transferred from interaction of charge particles in tissue result in radiative yields, and dose is predominantly locally deposited.

II: Compare particle tracks



1. e- mass much lower

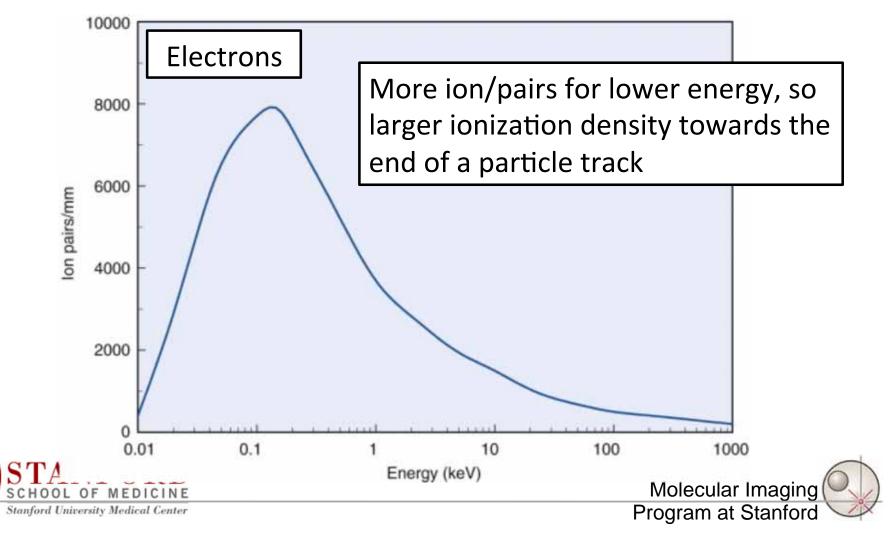
- 2. e- charge lower
- 3. e- experience large angle deflections (bremsstrahlung)
- Heavy charged particles travel in "straight lines, energy deposited locally
- Electrons undergo large angle deflections





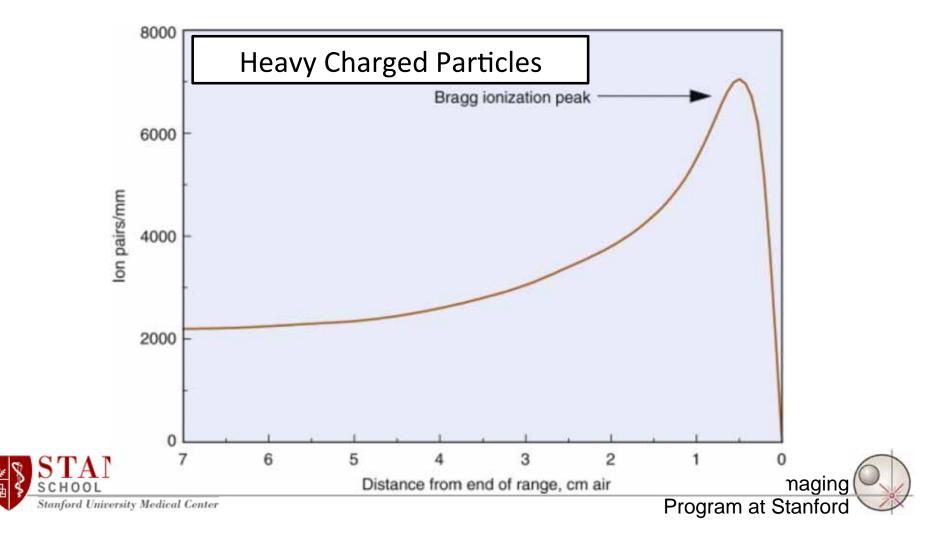
Specific ionization

- Specific ionization: number of ion pairs per distance
- The value is energy dependent



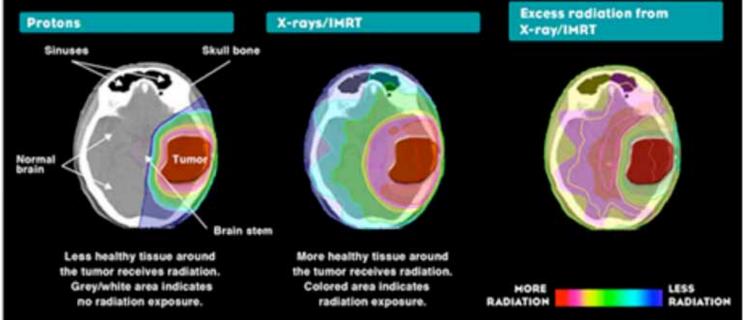
Specific ionization

- More energy deposited towards the end of track
- **Bragg Peak**, in particular for alpha particles



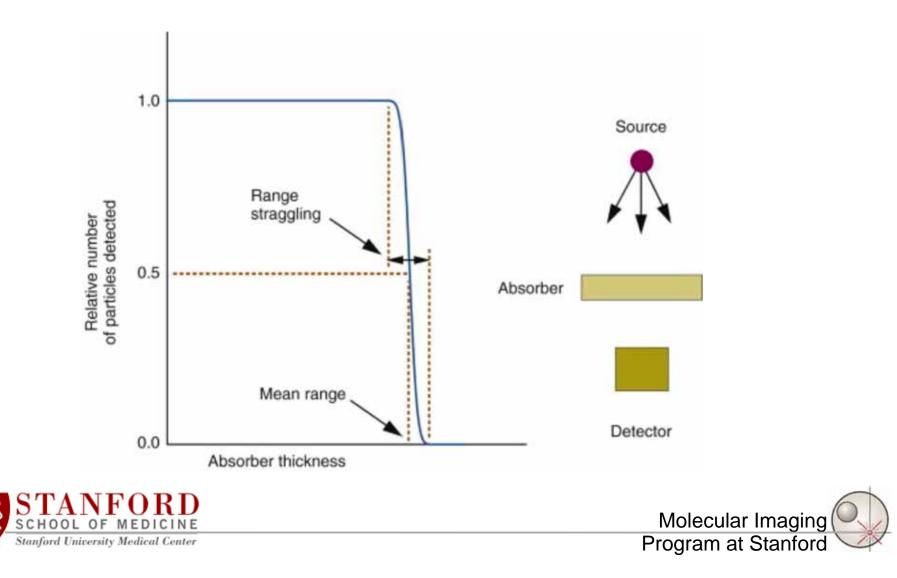
Proton Therapy





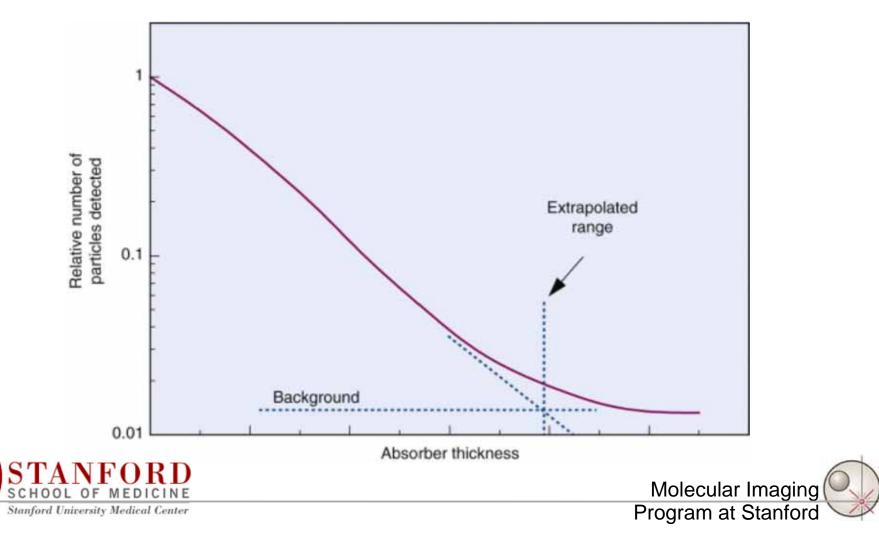
Particle Range

• Range of heavy particles (ex. Alpha particles & protons)



Particle Range

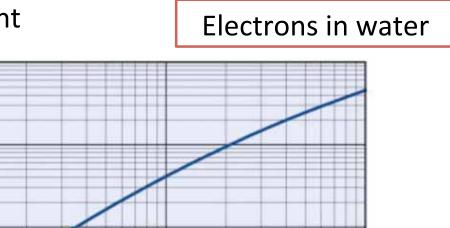
- Range of electrons/positrons
- More spread than heavy particles

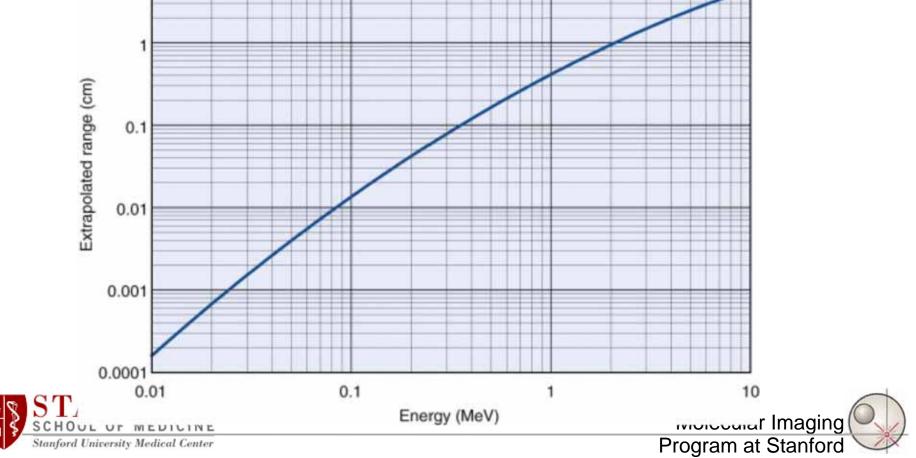


Particle Range

- Range of electrons/positrons
- Strongly energy dependent

10



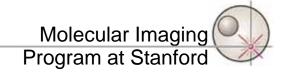


Stopping power and Range

	Material	Density	Stopping Power		Range			
		(g/cm ³)	MeV cm/g	(MeV/cm)	(g/cm²)	(cm)	(um)	
1 MeV proton	Air	0.00120	222	0.266	0.00287	2.39	23900	
1 MeV electron			1.66	0.00199	0.0490	408	408x10 ⁶	
1 MeV proton	Water	1.00	260	260	0.00246	0.00246	24.6	
1 MeV electron			1.85	1.85	0.437	0.437	4370	
1 MeV proton	Tungsten	19.3	63.5	1220	0.0122	0.00063	6.34	
1 MeV electron			1.02	19.6	0.768	0.0399	399	

- Density is crucial
- Stopping power decreases as Z/A
- Electrons about 2 orders of magnitude larger range
- Source NIST pstar and estar: http://physics.nist.gov/PhysRefData/Star/Text/ESTAR.html





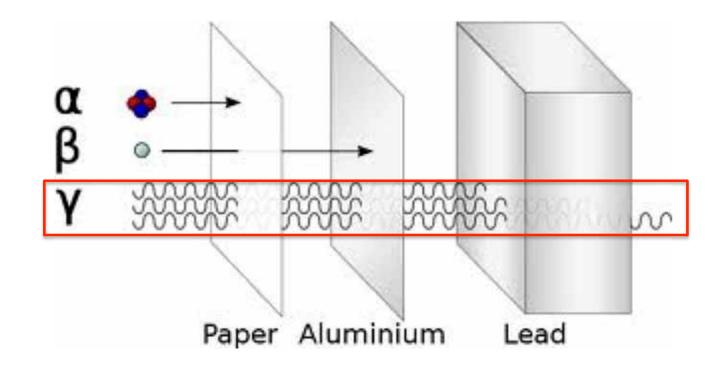
Heavy and Light Charged Particles: Takeaways

- Interaction of Radiation in Matter in two categories:
 - Charged Particles
 - Heavy Charged Particles
 - Electrons/Positions
- Also two primary energy transfer mechanisms for charged particles:
 - Collisional Energy Transfers
 - Inelastic Coulomb scattering
 - Elastic nuclear interactions
 - Radiative Energy Transfers
 - Bremsstrahlung





Photon Interactions



Photons are highly penetrating electromagnetic radiation





Interaction of radiation with matter

Distinction between three types:

- 1. Heavy charged particles:
 - Short, well defined range
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 - Rayleigh Scatter (non-ionizing)
 - Photo-electric Effect
 - Compton Scatter
 - Pair Production





Photon Interactions

• For a photon to deposit energy, energy needs to be transferred to an electron first

Two processes most relevant at Nuclear Medicine Energies:

- 1. Photoelectric absorption
- 2. Compton Scatter

Important: the electron that receives energy from the photon will deposit energy in the material (i.e. ionize the material)

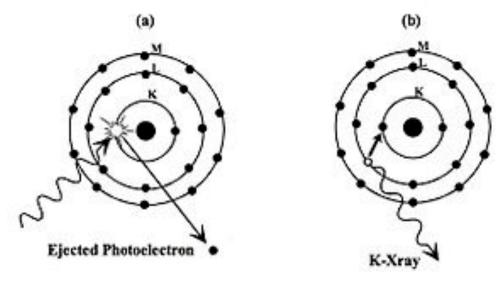




Photons: Photo-Electric Absorption

1. Photon absorbed by atom

- 2. Atom emits *photoelectron*, with energy:
 - $E_{pe} = E_v BE$ (BindingEnergy)
- 3. Photo-Electron now is ionizing
- 4. An higher shell electron fills the vacancy and emits an X-Ray photon







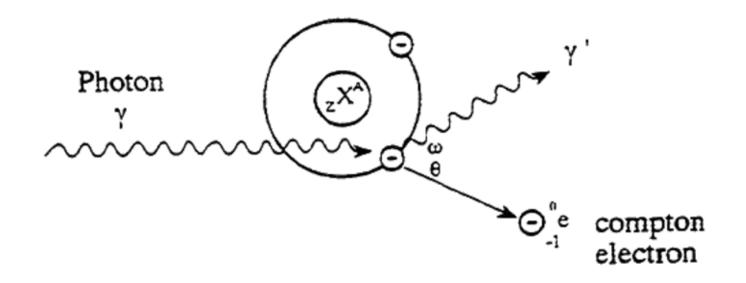
III: Photons: Compton Scatter

1. Photon scattered by electron

2. Electron overcomes the binding energy and gets ejected :

$$E_e = E_{\gamma} - E_{\gamma} - E_{binding}$$

3. Scattered -unbound- electron deposits energy







III: Photons: Compton Scatter

 $E_{\rm sc} = E_0 / [1 + (E_0 / 0.511) (1 - \cos \theta)]$

Photon Y

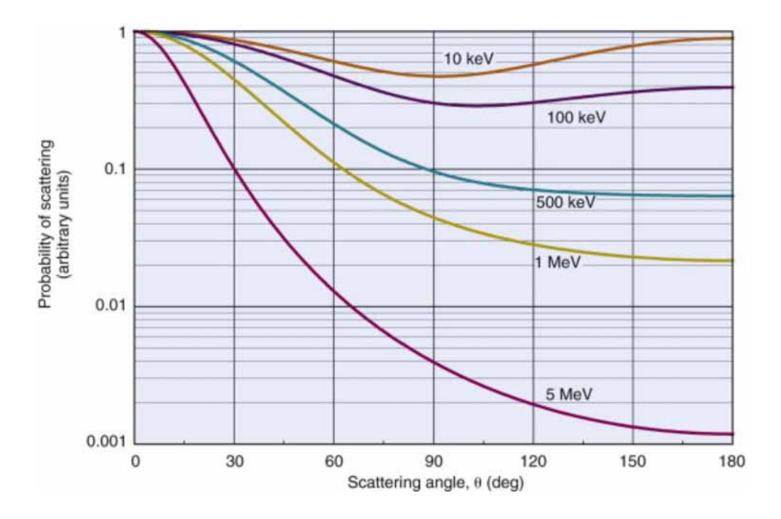
> [▲]⊖^e₋₁ compton electron

1. Photon scattered by electron

TABLE 6-2

SCATTERED PHOTON AND RECOIL ELECTRON ENERGIES FOR 180-DEGREE COMPTON SCATTERING INTERACTIONS

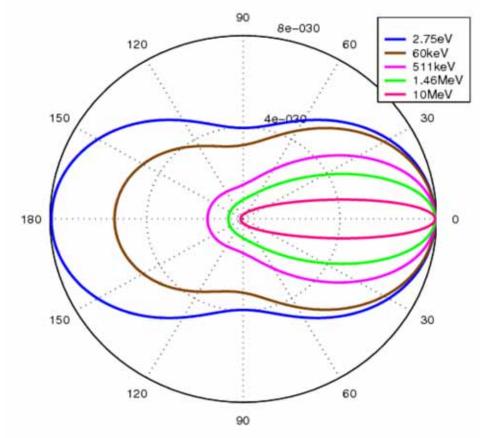
Radionuclide	Photon Energy (keV)	E_{sc}^{min} (keV)	E_{re}^{max} (keV)
125 I	27.5	24.8	2.7
¹³³ Xe	81	62	19
^{99m} Tc	140	91	49
$^{131}\mathrm{I}$	364	150	214
β^+ (annihilation)	511	170	341
⁶⁰ Co	1330	214	1116
—	~	255.5	—





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III: Photons: Compton Scatter



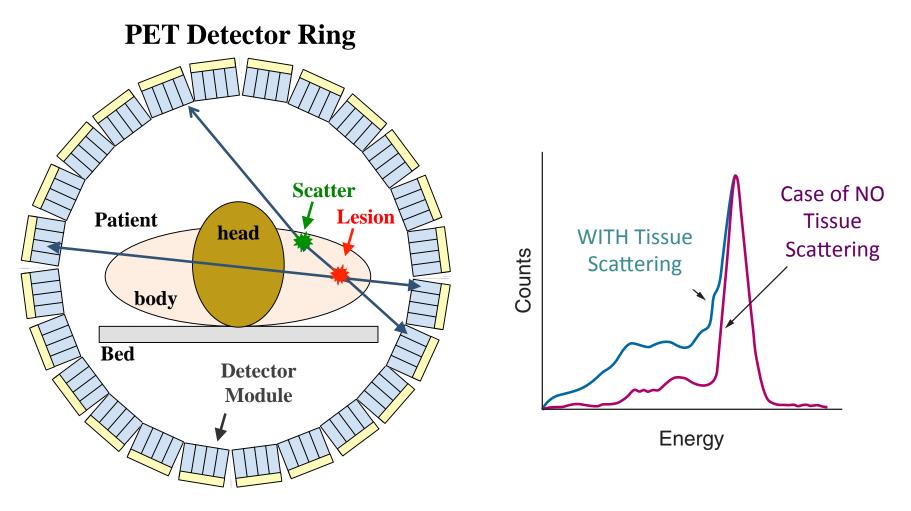
- Scatter more forward for higher energies
- Electron obtains most energy when photon backscatters (most energy transfer





How Angular Dependency Matters in PET

(One Example)

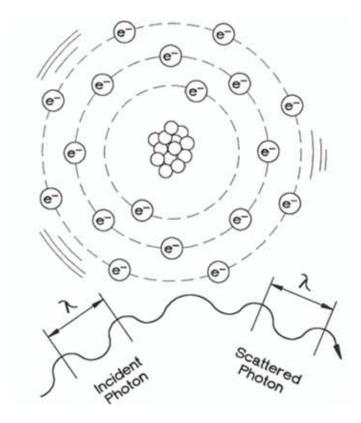




Molecular Imaging

Photons: Rayleigh Scatter

1. Elastic scatter of a photon off the entire atom



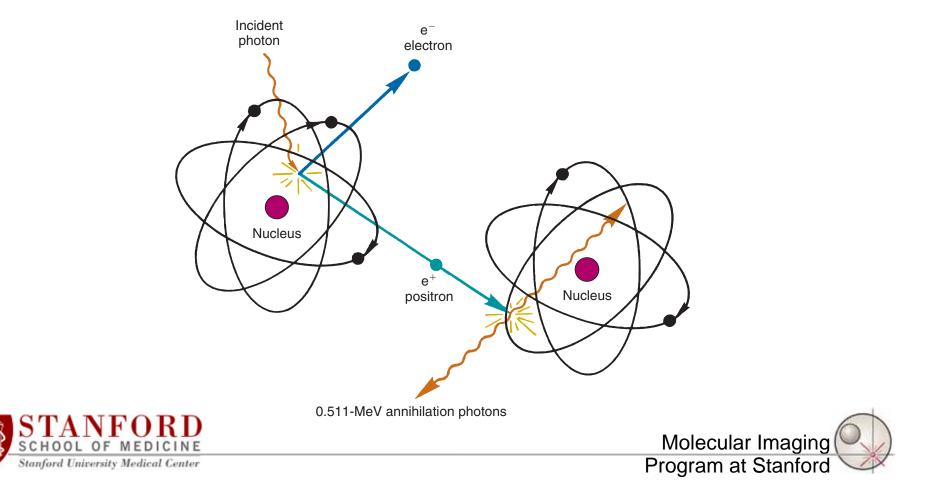
- 10 % of interactions at 30 keV (in soft tissue) - mammography
- 5 % of interactions at 70 keV (in soft tissue) - X-ray imaging
- Interaction probability goes up with ~Z³
- Non-ionizing!





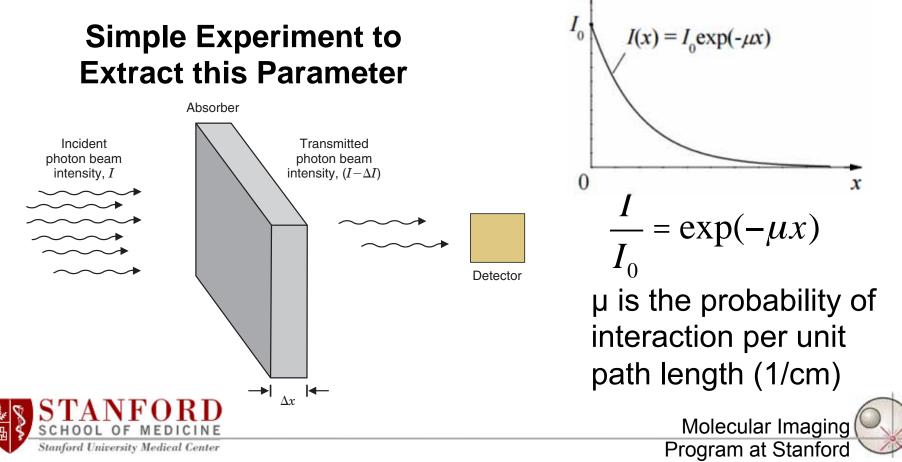
III: Photons: Other processes

 Pair production: higher energy photons are able to create electron-positron pairs (E>1.022 MeV), this process quickly becomes dominant (~ Z log(E))

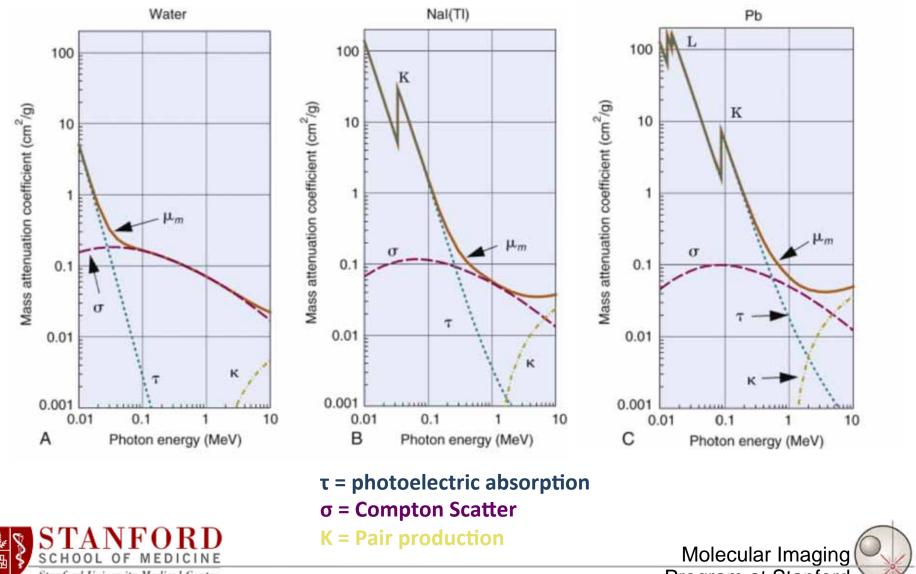


Photon interactions

- Interactions alter emissions from the radionuclide carefully selected for a molecular probe for imaging
- It is important to know how likely these interactions will affect emissions



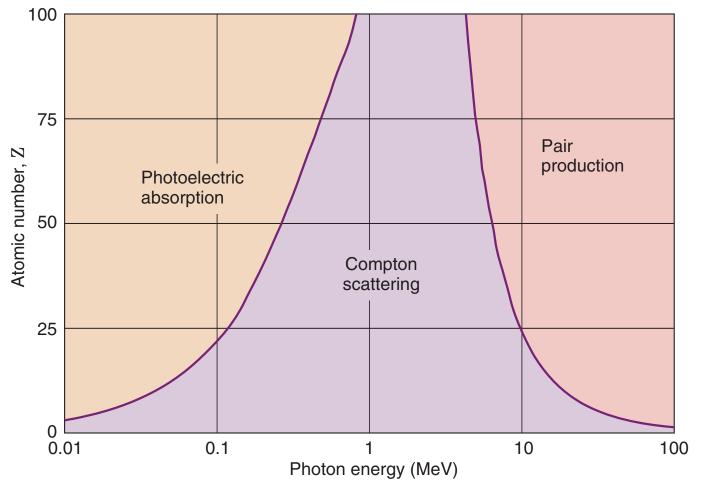
Photon Probability of Interaction



Stanford University Medical Center

Program at Stanford

Dominant Photon Interactions Z vs. E



Different processes dominant at different energies



Molecular Imaging

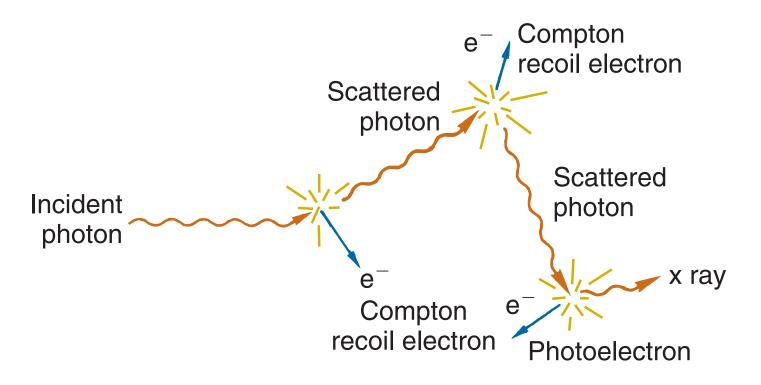
Photon interactions

- **Rayleigh Scatter:** coherent scatter whereby the photon changes direction, can be significant at low energies
- Photoelectric: γ -> photoelectron (-BE). Probability ~ Z⁴/E³
- **Compton Scatter**: $\gamma \rightarrow \gamma' + e'$. Probability ~ Z/E
- **Pair production:** higher energy photons are able to create electron-positron pairs (E>1.022 MeV), this process quickly becomes dominant (~ Z log(E))





How Photons Deposit Energy in Matter

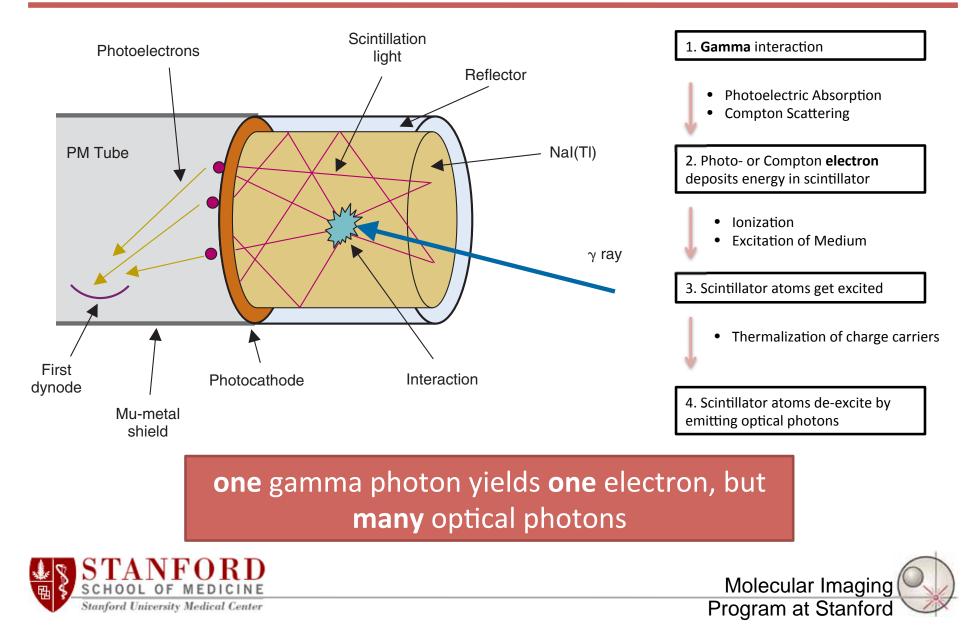


- Interactions of photons and charged particles with matter are coupled
- Secondary electrons ionize and deposit dose





A look forward: The Scintillation process



Photon interactions

		Air (ρ = 1.2 10 ⁻³ g/cm ³)			H ₂ 0 (ρ = 1 g/cm³)			Tungsten (ρ = 19 g/cm³)		
Energy		Attenuation	Mean free path	Total mean free path	Attenuation	Mean free path	e Total mean free path	Attenuation	Mean free path	Total mean free path
(keV)		(10 ⁻³ cm ² /g)	(10 ⁶ cm)	(cm)	(10 ⁻³ cm ² /g)	(10 ³ cm)	(cm)	(10 ⁻³ cm ² /g)	(cm)	(cm)
140	R	2.57	0.324	6030	2.79	0.358	6.51	100	0.519	0.0277
	С	135	0.006		150	0.007		98.5	0.528	
	PE	0.67	1.24		0.915	1.09		2000	0.031	
511	R	0.20	4.23	9640	0.22	4.65	10.4	9.14	5.68	0.388
	С	86.2	0.010		95.8	0.010		68.1	0.763	
	PE	0.01	64.4		0.02	56.2		56.6	0.918	
1000	R	0.05	16.2	13100	0.06	17.8	14.1	2.48	21.0	0.785
	С	63.6	0.013		70.7	0.0141		50.9	1.02	
	PE	0.003	311		0.004	2.72		12.8	4.06	

- Higher energy results in higher mean free path
- Mean free path = average distance between interactions
- Air almost no attenuation
- In water Compton dominant at E > 140 keV
- In tungsten Compton dominant at E > 500 keV



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 Z_{eff} air = 7.6 ; Z_{eff} H₂O = 7.4

