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**Concurrent- and after-effects of medial temporal lobe stimulation on directed
information flow to and from prefrontal and parietal cortices during memory
formation**

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Abstract

Electrical stimulation of the medial temporal lobe (MTL) has the potential to uncover causal circuit mechanisms underlying memory function. However, little is known about how MTL stimulation alters information flow with frontoparietal cortical regions implicated in episodic memory. We used intracranial electroencephalography recordings from humans (14 participants, 10 females) to investigate how MTL stimulation alters directed information flow between MTL and prefrontal cortex (PFC) and between MTL and posterior parietal cortex (PPC). Participants performed a verbal episodic memory task during which they were presented with words and asked to recall them after a delay of ~20 seconds. 50 Hz stimulation was applied to MTL electrodes on selected trials during memory encoding. Directed information flow was examined using phase transfer entropy. Behaviorally, we observed that MTL stimulation reduced memory recall. MTL stimulation decreased top-down PFC→MTL directed information flow during both memory encoding and subsequent memory recall, revealing aftereffects more than 20 seconds after end of stimulation. Stimulation suppressed top-down PFC→MTL influences to a greater extent than PPC→MTL. Finally, MTL→PFC information flow on stimulation trials was significantly lower for successful, compared to unsuccessful, memory recall; in contrast, MTL→ventral PPC information flow was higher for successful, compared to unsuccessful, memory recall. Together these results demonstrate that the effects of MTL stimulation are behaviorally, regionally, and directionally specific, that MTL stimulation selectively impairs directional signaling with PFC, and that causal MTL-ventral PPC circuits support successful memory recall. Findings provide new insights into dynamic casual circuits underling episodic memory and their modulation by MTL stimulation.

Significance Statement

The medial temporal lobe (MTL) and its interactions with prefrontal cortex (PFC) play a critical role in human memory. Dysfunctional MTL-PFC circuits are prominent in psychiatric and neurological disorders including Alzheimer's disease and schizophrenia. Brain stimulation has emerged as a potential mechanism for enhancing memory and cognitive functions, but the underlying neurophysiological mechanisms and dynamic causal circuitry underlying bottom-up and top-down signaling involving the MTL are unknown. Here, we use intracranial electroencephalography recordings to investigate the effects of MTL stimulation on causal signaling in key episodic memory circuits linking the MTL with PFC. Our findings have implications for translational applications aimed at realizing the promise of brain stimulation-based treatment of memory disorders.

144 **Introduction**

145
 146 The medial temporal lobe (MTL) and its interactions with prefrontal cortex (PFC) play a
 147 foundational role in human memory (Amer & Davachi, 2022; Cabeza, Ciaramelli, Olson, &
 148 Moscovitch, 2008; Curtis, 2006; Eichenbaum, 2017; Husain & Nachev, 2007; Rolls, 2018, 2019;
 149 Rutishauser, Reddy, Mormann, & Sarnthein, 2021; Vogt & Pandya, 1987; Wagner, Shannon,
 150 Kahn, & Buckner, 2005). Dysfunctional MTL-PFC circuits are prominent in psychiatric and
 151 neurological disorders including Alzheimer's disease and schizophrenia (Dickerson &
 152 Eichenbaum, 2010; Meyer-Lindenberg et al., 2005; Uhlhaas & Singer, 2012). Brain stimulation
 153 has emerged as a potential mechanism for enhancing memory function (Alagapan, Lustenberger,
 154 Hadar, Shin, & Fröhlich, 2019; Ezzyat et al., 2018; Fell et al., 2013; Kucewicz, Berry, Miller, et
 155 al., 2018; van der Plas, Braun, Stauch, & Hanslmayr, 2021; J. X. Wang et al., 2014; Yeh & Rose,
 156 2019) and cognitive function (Grover, Nguyen, & Reinhart, 2021; Ramirez-Zamora et al., 2020),
 157 but the underlying neurophysiological mechanisms and dynamic causal circuitry underlying
 158 bottom-up and top-down signaling involving the MTL are poorly understood. Given its critical
 159 role in memory formation, deep brain stimulation of the MTL with simultaneous recordings in
 160 the MTL and PFC has the potential to inform causal circuit mechanisms of encoding and recall
 161 in the human brain. Here, we use intracranial electroencephalography (iEEG) recordings to
 162 investigate the effects of MTL stimulation on causal signaling in key episodic memory circuits
 163 linking the MTL with PFC.

164

165 Electrophysiological studies in rodents have reported greater information flow from the MTL to
 166 the medial PFC than the reverse during spatial working memory (Zhang, Guo, & Liu, 2022). In
 167 non-human primates, MTL-dorsolateral and -ventrolateral PFC interactions have been linked

168 with memory performance (Brincat & Miller, 2015; Cruzado, Tiganj, Brincat, Miller, & Howard,
 169 2020). In humans, fMRI studies have consistently found coactivation of the MTL and multiple
 170 PFC regions during both spatial and verbal memory tasks (Dickerson & Eichenbaum, 2010;
 171 Dobbins, Foley, Schacter, & Wagner, 2002; M. Moscovitch, Cabeza, Winocur, & Nadel, 2016;
 172 Qin et al., 2014; Rugg & Vilberg, 2013; Simons & Spiers, 2003). Moreover, MTL-ventromedial
 173 PFC coactivation is also associated with better memory performance (Kumaran, Summerfield,
 174 Hassabis, & Maguire, 2009). Other studies have shown that functional connectivity between the
 175 MTL and medial PFC is also associated with memory recall (Preston & Eichenbaum, 2013; Qin
 176 et al., 2014; van Kesteren, Fernández, Norris, & Hermans, 2010). Furthermore, non-invasive
 177 magnetoencephalography studies in humans have suggested that coherence between the MTL
 178 and the superior frontal gyrus and medial PFC subdivisions in the delta-theta frequency band is
 179 associated with successful memory integration (Backus, Schoffelen, Szabéni, Hanslmayr, &
 180 Doeller, 2016; Guitart-Masip et al., 2013; Spaak & de Lange, 2020). iEEG studies in humans
 181 have reported increased MTL-dorsolateral and -ventrolateral PFC theta band synchronization
 182 during episodic memory encoding and recall compared to resting baseline conditions (Anderson,
 183 Rajagovindan, Ghacibeh, Meador, & Ding, 2010; Das & Menon, 2021; Ekstrom & Watrous,
 184 2014; Watrous, Tandon, Conner, Pieters, & Ekstrom, 2013).

185

186 Although prior non-invasive studies have provided significant insights into the role of the MTL
 187 and PFC in human episodic memory processing, the causal effects of brain stimulation on the
 188 electrophysiology of dynamic “bottom-up” and “top-down” interactions involving the PFC
 189 remains unknown. While non-invasive transcranial magnetic stimulation can be used to
 190 transiently alter neural processing in targeted cortical regions (J. X. Wang et al., 2014; Yeh &

191 Rose, 2019), it cannot precisely target deep brain structures such as the MTL (Kim, Ekstrom, &
192 Tandon, 2016; Rossini & Rossi, 2007). Intracranial electrical stimulation provides an alternative
193 approach that can more precisely map functional brain circuits (Mohan et al., 2020; Paulk et al.,
194 2022) and assess the neurophysiological basis of cognitive processes and its causal basis (Grover
195 et al., 2021; Huang & Keller, 2022; Mercier et al., 2022).

196

197 We recently found evidence for asymmetric frequency-specific feedforward and feedback
198 information flow between hippocampus and PFC during memory formation (Das & Menon,
199 2021). Specifically, we found higher directed information flow from the MTL to the PFC than
200 the reverse, in delta-theta frequency band and higher directed information flow from the PFC to
201 the MTL, than the reverse, in the beta frequency band (Das & Menon, 2021, 2022). Crucially,
202 these findings were observed during both memory encoding and recall periods, indicating a
203 prominent role of delta-theta for “bottom-up” signaling and beta for “top-down” signaling in the
204 cortex.

205

206 Here we use iEEG data from the UPENN-RAM consortium (Goyal et al., 2018; Jacobs et al.,
207 2016) to investigate how MTL stimulation alters directed information flow between the MTL
208 and the PFC during episodic memory processing. Participants were presented a list of words
209 during the encoding period and after a short delay, were asked to recall as many words as
210 possible from the list. During encoding, stimulation was applied at 50 Hz to select MTL
211 electrodes on alternate word pairs, and memory recall was probed after a ~20 second delay
212 period. The choice of 50 Hz stimulation frequency was motivated by its overlap with the gamma
213 band (30-80 Hz) which has been associated with human episodic memory and the amplitude of

214 iEEG fluctuations in this frequency band has been shown to reflect the underlying activity of
 215 single-neurons (Kahana, 2006; Kucewicz et al., 2014; Lachaux, Axmacher, Mormann, Halgren,
 216 & Crone, 2012). Moreover, previous studies have reported that MTL stimulation applied in the
 217 40-50 Hz range has a direct impact on memory performance (Fell et al., 2013; Inman et al.,
 218 2018; Suthana et al., 2012). We investigated how MTL stimulation alters its information flow
 219 with the PFC. We used phase transfer entropy (PTE) (Hillebrand et al., 2016; Lobier,
 220 Siebenhühner, Palva, & Matias, 2014; M. Y. Wang et al., 2017) which provides a robust and
 221 powerful measure for characterizing information flow between brain regions based on phase
 222 coupling and, crucially, it captures linear as well as nonlinear intermittent and nonstationary
 223 dynamics in iEEG data (Hillebrand et al., 2016; Lobier et al., 2014; Menon et al., 1996).

224

225 The main goal of our study was to investigate how MTL stimulation alters directed information
 226 flow between the MTL and the PFC. We build on our recent findings of asymmetric frequency-
 227 dependent directed information flow focused on the delta-theta (0.5-8 Hz) and beta (12-30 Hz)
 228 frequency bands (Das & Menon, 2021, 2022). Our analysis focused on the middle frontal gyrus
 229 (MFG) encompassing the dorsolateral PFC regions implicated in memory formation and
 230 monitoring (Chua & Ahmed, 2016; Rugg, 2022). We contrast this with MTL interactions with
 231 the inferior frontal gyrus (IFG) encompassing the ventrolateral PFC regions which has been
 232 implicated in controlled retrieval (Badre, Poldrack, Paré-Blagoev, Insler, & Wagner, 2005; Badre
 233 & Wagner, 2007; Dobbins et al., 2002; Hasegawa, Hayashi, & Miyashita, 1999; Wagner, Paré-
 234 Blagoev, Clark, & Poldrack, 2001).

235

236 The second goal of our study was to determine whether bottom-up and top-down information
 237 flow between the MTL and the PFC and posterior parietal cortex (PPC) are similarly impacted
 238 by MTL stimulation. Multiple lines of evidence across species have revealed a role for the PPC
 239 in episodic memory (Cabeza, 2008; Cabeza, Ciaramelli, & Moscovitch, 2012; Cabeza et al.,
 240 2008; Cabeza et al., 2011; Hutchinson, Uncapher, & Wagner, 2009; Uncapher & Wagner, 2009;
 241 Wagner et al., 2005). Anterograde and retrograde tracing studies in non-human primates have
 242 uncovered projections from the MTL to the PPC (Clower, West, Lynch, & Strick, 2001; Insausti
 243 & Muñoz, 2001) and in the reverse direction (Rockland & Van Hoesen, 1999). Single-neuron
 244 studies in rodents (Chen, Lin, Green, Barnes, & McNaughton, 1994; McNaughton et al., 1994;
 245 Nitz, 2006) as well as non-human primates (Andersen, Essick, & Siegel, 1985; Crowe, Chafee,
 246 Averbach, & Georgopoulos, 2004) have established PPC involvement in spatial memory. fMRI
 247 studies in non-human primates have reported coactivation of the MTL and PPC during
 248 successful memory encoding and recall (Miyamoto et al., 2013).
 249
 250 Studies using resting-state fMRI in humans have confirmed intrinsic MTL connectivity with the
 251 PPC (Vincent et al., 2006). Other human fMRI studies have reported dorsal PPC activation
 252 during episodic memory retrieval (Buckner et al., 1998; Konishi, Wheeler, Donaldson, &
 253 Buckner, 2000), spatial memory processing (Amorapanth, Widick, & Chatterjee, 2010;
 254 Baumann, Chan, & Mattingley, 2012), and coactivation of the hippocampus and multiple
 255 subdivisions of the PPC during episodic and semantic memory encoding and retrieval
 256 (Ciaramelli, Burianová, Vallesi, Cabeza, & Moscovitch, 2020; Gurd et al., 2002; Vincent et al.,
 257 2006). The dorsal PPC is involved in top-down attention processing during memory encoding
 258 (Cabeza, 2008; Cabeza et al., 2012; Cabeza et al., 2011; Ciaramelli, Grady, & Moscovitch, 2008;

259 Daselaar et al., 2009; Hutchinson et al., 2009; Uncapher & Wagner, 2009). Human
 260 electrocorticography studies have suggested a role for the PPC in verbal episodic memory
 261 encoding and recall (Gonzalez et al., 2015) and human iEEG studies have found that
 262 hippocampus-PPC correlation in the theta frequency band is prominent in spatial memory
 263 (Ekstrom et al., 2005). Together, these findings suggest that coordinated interactions between the
 264 MTL and PPC play a role in episodic memory. However, the causal role of MTL-PPC circuits
 265 remains poorly understood and it is not known whether MTL stimulation alters directed
 266 information flow between MTL and PPC differently from the PFC.

267

268 Our analyses reveal how MTL stimulation alters frequency-specific bottom-up and top-down
 269 information flow between the MTL and PFC and how this differs from PPC regions implicated
 270 in human episodic memory. Findings provide new insights into causal mechanisms involved in
 271 the operation of human episodic memory circuits.

272

273 **Materials and Methods**

274 ***UPENN-RAM iEEG recordings***

275

276 iEEG recordings from 14 patients (10 females, 4 males) shared by Kahana and colleagues at the
 277 University of Pennsylvania (UPENN) (obtained from the UPENN-RAM public data release)
 278 were used for analysis (Goyal et al., 2018; Jacobs et al., 2016). Patients with pharmaco-resistant
 279 epilepsy underwent surgery for removal of their seizure onset zones. iEEG recordings of these
 280 patients were downloaded from a UPENN-RAM consortium hosted data sharing archive (URL:
 281 <http://memory.psych.upenn.edu/RAM>). Prior to data collection, research protocols and ethical
 282 guidelines were approved by the Institutional Review Board at the participating hospitals and

283 informed consent was obtained from the participants and guardians (Jacobs et al., 2016). Details
 284 of all the recordings sessions and data pre-processing procedures are described by Kahana and
 285 colleagues (Jacobs et al., 2016). Briefly, iEEG recordings were obtained using subdural grids and
 286 strips (contacts placed 10 mm apart) or depth electrodes (contacts spaced 5–10 mm apart) using
 287 recording systems at each clinical site. iEEG systems included DeltaMed XiTek (Natus), Grass
 288 Telefactor, and Nihon-Kohden EEG systems. These patients performed a verbal episodic
 289 memory task (see below) and received direct brain stimulation during some of the encoding
 290 trials. Electrodes located in brain lesions or those which corresponded to seizure onset zones or
 291 had significant interictal spiking or had broken leads, were excluded from analysis.

292

293 Anatomical localization of electrode placement was accomplished by co-registering the
 294 postoperative computed CTs with the postoperative MRIs using FSL (FMRIB (Functional MRI
 295 of the Brain) Software Library), BET (Brain Extraction Tool), and FLIRT (FMRIB Linear Image
 296 Registration Tool) software packages. Preoperative MRIs were used when postoperative MRIs
 297 were not available. The resulting contact locations were mapped to MNI space using an indirect
 298 stereotactic technique and OsiriX Imaging Software DICOM viewer package. We used the
 299 Brainnetome atlas (Fan et al., 2016) to demarcate bihemispheric middle and inferior frontal
 300 gyrus subdivisions of the prefrontal cortex (MFG and IFG) and dorsal and ventral subdivisions
 301 of the posterior parietal cortex (dPPC and vPPC) as well as the hippocampus, parahippocampal
 302 gyrus, and entorhinal cortex subdivisions of the MTL. We first identified electrode pairs in
 303 patients with electrodes implanted in each pair of brain regions of interest (for example, MTL-
 304 MFG). Key PPC regions of interest included the superior parietal lobule, and supramarginal
 305 gyrus, intraparietal sulcus and angular gyrus in the inferior parietal lobule, spanning its dorsal-

306 ventral axis. The lack of sufficient number of participants and electrode pairs precluded analyses
 307 of these subdivisions separately. We therefore combined electrodes from the superior parietal
 308 lobule, intraparietal sulcus, and supramarginal gyrus into a dorsal PPC subdivision and the
 309 angular gyrus regions into a ventral PPC subdivision (**Tables 2, 3**). Ages of these patients ranged
 310 from 20 to 49, with mean age 36.0 ± 10.1 and the dataset included 10 females. Gender
 311 differences were not analyzed in this study due to lack of sufficient male participants for
 312 electrodes pairs for MTL-MFG, MTL-IFG, MTL-dPPC, and MTL-vPPC interactions (**Table 2**).
 313
 314 Original sampling rates of iEEG signals were 500 Hz, 1000 Hz, and 1600 Hz. Hence, iEEG
 315 signals were downsampled to 500 Hz, if the original sampling rate was higher, for all subsequent
 316 analysis. The two major concerns when analyzing interactions between closely spaced
 317 intracranial electrodes are volume conduction and confounding interactions with the reference
 318 electrode (Burke et al., 2013). Hence bipolar referencing was used to eliminate confounding
 319 artifacts and improve the signal-to-noise ratio of the neural signals, consistent with previous
 320 studies using UPENN-RAM iEEG data (Burke et al., 2013; Ezzyat et al., 2018). Signals recorded
 321 at individual electrodes were converted to a bipolar montage by computing the difference in
 322 signal between adjacent electrode pairs on each strip, grid, and depth electrode and the resulting
 323 bipolar signals were treated as new “virtual” electrodes originating from the midpoint between
 324 each contact pair, identical to procedures in previous studies using UPENN-RAM data (Solomon
 325 et al., 2019). Line noise (60 Hz) and its harmonics were removed from the bipolar signals and
 326 finally each bipolar signal was Z-normalized by removing mean and scaling by the standard
 327 deviation. For filtering, we used a fourth order two-way zero phase lag Butterworth filter
 328 throughout the analysis.

329

330 *iEEG verbal free recall task and stimulation paradigm*

331

332 Patients performed multiple trials of a free recall experiment, where they were presented with a
 333 list of words and subsequently asked to recall as many as possible from the original list (**Figure**
 334 **1c**) (Solomon et al., 2017; Solomon et al., 2019). Each session consisted of 25 lists. The task
 335 consisted of three periods: encoding, delay, and recall. During encoding, a list of 12 words was
 336 visually presented for ~30 sec. Words were selected at random, without replacement, from a pool
 337 of high frequency English nouns (http://memory.psych.upenn.edu/Word_Pools). Each word was
 338 presented for a duration of 1600 msec, followed by an inter-stimulus interval of 800 to 1200
 339 msec. After a 20 sec post-encoding delay where participants performed a series of distractor
 340 tasks consisting of arithmetic problems of the form $a+b+c=?$, where a , b , and c were randomly
 341 chosen integers from 1 to 9, participants were instructed to recall as many words as possible
 342 during the 30 sec recall period.

343

344 For each subject, a selected electrode pair in the MTL was connected to an electrical stimulator
 345 (Grass Technologies or Blackrock Microsystems) and stimulation was applied using parameters
 346 from a prior study (Suthana et al., 2012), showing a positive effect of stimulation on memory
 347 performance. Subjects were instructed about the stimulation procedure but were blinded to the
 348 location of the stimulation sites. Bipolar-symmetric, charge-balanced, square-wave stimulation
 349 current between a pair of electrodes was applied at 50 Hz and 300 μ s pulse-width. All the
 350 stimulation electrodes in the present study were depth electrodes. Safe amplitude for stimulation
 351 was determined at the start of each session under a clinically supervised mapping procedure by

352 manually testing a range of currents for each site, beginning at 0.25 mA and slowly increasing to
353 a maximum of 1.5 mA. The final stimulation current (**Table 1**) that was used for the cognitive
354 experiments was the maximum current for each site that could be applied without inducing
355 patient symptoms, epileptiform after discharges, or seizures. We designated a stimulation site
356 being in the MTL if at least one electrode of the bipolar pair was in the region.

357
358 For the stimulated lists, exactly half of the words on the list were delivered simultaneously with
359 electrical brain stimulation. For the control lists, all 12 words on the list were presented without
360 stimulation. Out of the 25 lists in each session, 20 were stimulated lists and 5 were control lists in
361 a randomly assigned order. For each stimulated list, stimulation occurred in a blocked pattern:
362 the stimulator was active during the presentation of a pair of consecutive words and then inactive
363 for the following pair. Thus, in total, on each stimulated list, the stimulator was active for half
364 the total words. For the stimulation blocks, the stimulator was timed to occur 200 msec before
365 the presentation of the first word in each block, continuing for 4.6 s, until the disappearance of
366 the second word. The onset of stimulation was balanced, such that a random half of the
367 stimulation lists began with a non-stimulated block and the others began with a stimulated block.

368
369 We analyzed 1600 msec iEEG epochs from the encoding periods of the free recall task. For the
370 recall periods, iEEG recordings 1600 msec prior to the vocal onset of each word were analyzed
371 (Solomon et al., 2019). Data from each trial was analyzed separately and specific measures were
372 averaged across trials. Effects of electrical stimulation on behavioral performance has been
373 analyzed in detail by Kahana and colleagues elsewhere (Goyal et al., 2018; Jacobs et al., 2016).
374 Our major focus in this study was on the effect of stimulation on the direction of information

375 flow between the MTL and the PFC and PPC. The mismatch in the number of trials between
 376 successfully versus unsuccessfully encoded words (roughly 1:3) made it difficult to directly
 377 compare causal signaling measures associated with the two. From the point of view of probing
 378 behaviorally effective memory encoding, our focus was therefore on how MTL stimulation
 379 affects successful encoding and recall, consistent with most prior studies (Long, Burke, &
 380 Kahana, 2014; Watrous et al., 2013). For stimulation trials, data corresponding to the pair of
 381 words immediately succeeding the stimulated word pair was analyzed. Data corresponding to the
 382 stimulated word pair were excluded from analysis to prevent contamination with stimulation
 383 artifact (Hansen et al., 2018; Jun, Lee, Kim, Jeong, & Chung, 2020; Kucewicz, Berry, Miller, et
 384 al., 2018).

385

386 *Control analysis using resting-state iEEG data with MTL stimulation*

387

388 For the control condition, we used “resting-state” data from 2 participants collected in the
 389 UPENN-RAM public data release (Solomon et al., 2021). These patients were part of a larger
 390 “parameter search” project whose major goal was to systematically study the effects of
 391 stimulation frequency, current, and stimulation brain regions (Mohan et al., 2020). We
 392 reanalyzed iEEG data from these participants to determine whether the main findings of directed
 393 information flow between the MTL and the PFC and PPC in our study were due to brain
 394 stimulation causing reorganization of brain circuits and thus influencing the information flow
 395 that we observed in the memory task. Similar to the memory task, bipolar-symmetric, charge-
 396 balanced, square-wave stimulation current between a pair of depth MTL electrodes was applied
 397 at 50 Hz and 300 μ s pulse-width (also see **Table 6**). Similar procedures were adopted for

determining the safe current amplitude for stimulation for these participants. Based on electrode placement in the MTL and the PFC and PPC brain regions and based on the criteria that the stimulation frequency was 50 Hz, we selected 2 subjects with simultaneous electrode placements in MTL and MFG (100 electrode pairs) and also MTL and dPPC (60 electrode pairs). IFG and vPPC were excluded from analysis due to lack of electrode placements in these regions. The stimulation duration for these two subjects were 250 msec and 500 msec (**Table 6**).

We analyzed 1600 msec iEEG epochs immediately prior to the start of each stimulation trial; these correspond to the “non-stim” condition. We also analyzed 1600 msec iEEG epochs immediately after the end of each stimulation trial; these correspond to the “stim” condition. Trials were spaced by 3 s, with up to ± 200 msec of randomly-applied jitter added to the interval. Subjects were instructed to sit quietly and did not perform any task. Similar to the memory task, data from each trial was analyzed separately and PTE measures were averaged across trials. Data corresponding to the stimulated epochs were excluded from analysis to prevent contamination with stimulation artifact (Hansen et al., 2018; Jun et al., 2020; Kucewicz, Berry, Miller, et al., 2018).

iEEG analysis of power

For power analysis, we first filtered the signals in the delta-theta (0.5-8 Hz) and beta (12-30 Hz) frequency bands and then calculated the square of the filtered signals as the power of the signals (Kwon et al., 2021). Signals were then smoothed using 0.2 sec windows with 90% overlap (Kwon et al., 2021) and normalized with respect to 0.2 sec pre-stimulus periods.

iEEG analysis of phase transfer entropy (PTE) and direction of information flow

Phase transfer entropy (PTE) is a nonlinear measure of the directionality of information flow between time-series and can be applied to nonstationary time-series (Das & Menon, 2020; Lobier et al., 2014). Note that information flow described here relates to signaling between brain areas and does not necessarily reflect the representation or coding of behaviorally relevant variables per se. The PTE measure is in contrast to the Granger causality measure which can be applied only to stationary time-series (Barnett & Seth, 2014). We first carried out a stationarity test of the iEEG recordings (unit root test for stationarity (Barnett & Seth, 2014)) and found that the spectral radius of the autoregressive model is very close to one, indicating that the iEEG time-series is nonstationary. This precluded the applicability of the Granger causality analysis in our study.

Given two time-series $\{x_i\}$ and $\{y_i\}$, where $i = 1, 2, \dots, M$, instantaneous phases were first extracted using the Hilbert transform. Let $\{x_i^p\}$ and $\{y_i^p\}$, where $i = 1, 2, \dots, M$, denote the corresponding phase time-series. If the uncertainty of the target signal $\{y_i^p\}$ at delay τ is quantified using Shannon entropy, then the PTE from driver signal $\{x_i^p\}$ to target signal $\{y_i^p\}$ can be given by

$$PTE_{x \rightarrow y} = \sum_i p(y_{i+\tau}^p, y_i^p, x_i^p) \log \left(\frac{p(y_{i+\tau}^p | y_i^p, x_i^p)}{p(y_{i+\tau}^p | y_i^p)} \right), \quad (i)$$

where the probabilities can be calculated by building histograms of occurrences of singles, pairs, or triplets of instantaneous phase estimates from the phase time-series (Hillebrand et al., 2016).

443 For our analysis, the number of bins in the histograms was set as $3.49 \times STD \times M^{-1/3}$ and delay τ
 444 was set as $2M/M_{\pm}$, where STD is average standard deviation of the phase time-series $\{\phi_i^p\}$ and $\{\psi_i^p\}$
 445 and M_{\pm} is the number of times the phase changes sign across time and channels (Hillebrand et
 446 al., 2016). PTE has been shown to be robust against the choice of the delay τ and the number of
 447 bins for forming the histograms (Hillebrand et al., 2016).

449 *iEEG analysis of phase locking value (PLV) and phase synchronization*

450
 451 We used phase locking value (PLV) to compute phase synchronization between two time-series
 452 (Lachaux, Rodriguez, Martinerie, & Varela, 1999). We first calculated the instantaneous phases
 453 of the two signals by using the analytical signal approach based on the Hilbert transform (Bruns,
 454 2004). Given time-series $x(t)$, $t = 1, 2, \dots, M$, its complex-valued analytical signal $z(t)$ can be
 455 computed as

$$456 \quad z(t) = x(t) + i\hat{x}(t) = A_x(t)e^{i\Phi_x(t)}, \quad (i)$$

458
 459 where i denotes the square root of minus one, $\hat{x}(t)$ is the Hilbert transform of $x(t)$, and $A_x(t)$ and
 460 $\Phi_x(t)$ are the instantaneous amplitude and instantaneous phase respectively and can be given by

$$461 \quad A_x(t) = \sqrt{[x(t)]^2 + [\hat{x}(t)]^2} \quad \text{and} \quad \Phi_x(t) = \arctan \frac{\hat{x}(t)}{x(t)}. \quad (ii)$$

463
 464 The Hilbert transform of $x(t)$ was computed as

465

466

$$\hat{x}(t) = \frac{1}{\pi} PV \int_{-\infty}^{\infty} \frac{x(\tau)}{t-\tau} d\tau, \quad (\text{iii})$$

467

468 where PV denotes the Cauchy principal value. MATLAB function “hilbert” was used to469 calculate the Hilbert transform in our analysis. Given two time-series $x(t)$ and $y(t)$, where470 $t = 1, 2, \dots, M$, the PLV (zero-lag) can be computed as

471

472

$$PLV @ \left| E \left[e^{i(\Phi_x(t) - \Phi_y(t))} \right] \right|, \quad (\text{iv})$$

473

474 where $\Phi_y(t)$ is the instantaneous phase for time-series $y(t)$, $||$ denotes the absolute value operator,475 $E[\cdot]$ denotes the expectation operator with respect to time t , and i denotes the square root of

476 minus one. PLVs were then averaged across trials to estimate the final PLV for each pair of

477 electrodes.

478

479 ***iEEG analysis of modulation index and phase-amplitude coupling (PAC)***

480

481 We used the modulation index estimation procedure (Tort et al., 2008) to calculate phase-

482 amplitude coupling (PAC) of electrodes. We first denote the amplitude and the phase frequency

483 ranges for our analysis by f_A ([80, 160] Hz) and f_P ([0.5, 8] Hz), respectively. Let $x(t)$ denote the484 time-series of the electrode. We first filter $x(t)$ at the two frequency ranges f_A and f_P . Let's denote485 the filtered signals as $x_{f_A}(t)$ and $x_{f_P}(t)$ respectively. We then estimate the phase time-series $\varphi_{f_P}(t)$ 486 from the Hilbert transform of $x_{f_P}(t)$ and the amplitude time-series $A_{f_A}(t)$ from the Hilbert

487 transform of $x_{fA}(t)$. Each point in the composite time-series $[\varphi_{fp}(t), A_{fA}(t)]$ indicates an
 488 amplitude of an oscillation in f_A at the corresponding phase in the fp oscillation. We next bin the
 489 phases $\varphi_{fp}(t)$ into eighteen 20° intervals (0° to 360°) and calculate the mean of A_{fA} over each
 490 of the phase bins. Let's $\langle A_{fA} \rangle_{\varphi_{fp}(j)}$ denote the mean A_{fA} value at each phase bin j . We then
 491 define entropy H as

$$H = - \sum_{j=1}^N p_j \log p_j ,$$

494
 495 where $N = 18$ is the number of phase bins and p_j is given by

$$p_j = \frac{\langle A_{fA} \rangle_{\varphi_{fp}(j)}}{\sum_{j=1}^N \langle A_{fA} \rangle_{\varphi_{fp}(j)}}.$$

498
 499 The MI is estimated by normalizing H by the maximum possible entropy value H_{max} which is
 500 obtained for the uniform distribution $p_j = 1/N$ ($H_{max} = \log N$):

$$MI = \frac{H_{max} - H}{H_{max}}.$$

502
 503 Higher MI values indicate stronger PAC with zero MI corresponding to zero PAC.

508 *Statistical analysis*

509

510 Statistical analysis was conducted using mixed effects analysis with the *lmerTest* package
 511 (Kuznetsova, Brockhoff, & Christensen, 2017) implemented in R software (version 4.0.2, R
 512 Foundation for Statistical Computing). Because PTE data were not normally distributed, we used
 513 BestNormalize (Peterson & Cavanaugh, 2018) which contains a suite of transformation-
 514 estimating functions that can be used to optimally normalize data. The resulting normally
 515 distributed data were subjected to mixed effects analysis with the following model: $PTE \sim$
 516 $Condition + (1|Subject)$, where *Condition* models the fixed effects (condition differences) and
 517 $(1|Subject)$ models the random repeated measurements within the same participant. Analysis of
 518 variance (ANOVA) was used to test the significance of findings with FDR-corrections for
 519 multiple comparisons ($p < 0.05$). Analysis of power, PLV, and PAC were carried out in the same
 520 manner using the mixed effects analysis.

521

522 The differential effects of stimulation on directed information flow between the MTL and the
 523 MFG, IFG, dPPC, and vPPC was also tested with a 2-way ANOVA with the factors Region
 524 (MFG, IFG, dPPC, and vPPC) and Stimulation (ON/OFF). Linear mixed effects analysis was run
 525 in a similar way, with the following model: $PTE \sim Stimulation \times Region + (1|Subject)$. 2-way
 526 ANOVA was then used to test the significance of findings with FDR-corrections for multiple
 527 comparisons ($p < 0.05$).

528

529 For effect size estimation, we used η^2 statistics for complex F-based effects such as interactions
 530 effects and main effects with multiple factors and Cohen's *d* statistics for pairwise post-hoc

531 comparisons. We used the *eta_squared()* function in the *effectsize* package implemented in R for
 532 estimating η^2 and the *lme.dscore()* function in the *EMAtools* package in R for estimating
 533 Cohen's *d*.

534

535 We also conducted surrogate analysis to test the significance of the estimated PTE values
 536 (Hillebrand et al., 2016). The estimated phases from the Hilbert transform for electrodes from a
 537 given pair of brain areas were time-shuffled so that the predictability of one time-series from
 538 another is destroyed, and PTE analysis was repeated on this shuffled data to build a distribution
 539 of surrogate PTE values against which the observed PTE was tested ($p < 0.05$).

540

541 **Results**

542

543 *Behavioral effects of MTL stimulation*

544

545 Participants were presented with a sequence of words and asked to remember them for
 546 subsequent recall (**Methods, Tables 1-3, Figure 1**) (Solomon et al., 2019). During encoding, a
 547 list of 12 words was visually presented for ~30 s. Each word was presented for a duration of
 548 1600 msec, followed by an inter-stimulus interval of 800 to 1200 msec. After a ~20 sec post-
 549 encoding delay, participants were instructed to recall as many words as possible from the
 550 original list during the 30 sec recall period. MTL stimulation occurred in a blocked pattern: the
 551 stimulator was active during the presentation of a pair of consecutive words and then inactive for
 552 the following pair.

553

554 Average memory recall accuracy across patients was $22.9\% \pm 11.7\%$ for MTL stimulation trials
 555 and $27.5\% \pm 12.9\%$ for non-stimulation trials. Memory recall was lower on stimulation,

556 compared to non-stimulation, trials, this difference was marginally significant ($p = 0.0574$,
 557 Cohen's $d = 0.51$, Wilcoxon signed-rank test). This result is consistent with prior studies using
 558 UPENN-RAM data (Goyal et al., 2018; Jacobs et al., 2016; Kucewicz, Berry, Kremen, et al.,
 559 2018) as well as other reports that direct stimulation of the hippocampus generally impairs
 560 memory (Chua & Ahmed, 2016; Coleshill et al., 2004; Fernandez, Hufnagel, Helmstaedter,
 561 Zentner, & Elger, 1996; Halgren, Wilson, & Stapleton, 1985; Herweg, Solomon, & Kahana,
 562 2020; Jackson, Feredoes, Rich, Lindner, & Woolgar, 2021; Jun et al., 2020; Lacruz et al., 2010;
 563 Merkow et al., 2017).

564

565 *Effect of MTL stimulation on information flow from MTL to PFC and PPC during memory*
 566 *encoding*

567

568 We examined the differential effects of stimulation on directed information flow from the MTL
 569 to MFG, IFG, dorsal PPC (dPPC), and ventral PPC (vPPC), using a 2-way ANOVA with the
 570 factors Region (MFG, IFG, dPPC, and vPPC) and Stimulation (ON/OFF) (**Methods**). We
 571 focused on directed information flow from the MTL to the PFC and PPC, in the delta-theta and
 572 beta bands, based on our replicable findings across verbal and spatial memory domains (Das &
 573 Menon, 2021, 2022). To preclude confounding influences associated with unsuccessful recall,
 574 we focused on how MTL stimulation affects encoding and recall on successful trials, consistent
 575 with prior studies (Long et al., 2014; Watrous et al., 2013). We found no interaction between
 576 Stimulation and Region in either delta-theta ($F(1, 660) = 0.06, p > 0.05, \eta^2 = 9.76\text{e-}05$) or beta
 577 ($F(1, 663) = 0.68, p > 0.05, \eta^2 = 1.02\text{e-}03$) frequency bands during memory encoding. We also
 578 did not find any main effects of Stimulation in either delta-theta ($F(1, 660) = 3.99, p > 0.05, \eta^2 =$

579 6.01e-03) or beta ($F(1, 663) = 0.06, p > 0.05, \eta^2 = 9.76\text{e-}05$) frequency bands during memory
 580 encoding (**Table 4**).

581

582 *Effect of MTL stimulation on information flow to the MTL from the PFC and PPC during*

583 *memory encoding*

584

585 We next examined directed information flow to the MTL from the PFC and PPC during verbal
 586 memory encoding. We examined the differential effects of stimulation on directed information
 587 flow from the MFG, IFG, dPPC, and vPPC to the MTL, using a 2-way ANOVA with factors
 588 Region (MFG, IFG, dPPC, and vPPC) and Stimulation (ON/OFF) (**Methods**). We found a
 589 significant Stimulation x Region interaction for directed information flow from the PFC and PPC
 590 to the MTL in the delta-theta band, ($F(1, 663) = 11.75, p < 0.01, \eta^2 = 0.02$) (**Table 4**). There was
 591 no interaction between Stimulation and Region ($F(1, 663) = 0.67, p > 0.05, \eta^2 = 1.01\text{e-}03$), or
 592 main effect of Stimulation ($F(1, 663) = 1.04, p > 0.05, \eta^2 = 1.57\text{e-}03$) in the beta frequency band
 593 (**Table 4**).

594

595 Next, we conducted post-hoc tests to systematically investigate regional differences in the effects
 596 of MTL stimulation on directed information flow to the MTL in the delta-theta band (**Figure 2**).

597 MFG→MTL directed information flow decreased during stimulation trials compared to non-
 598 stimulation trials in the delta-theta band ($F(1, 260) = 12.00, p < 0.01$, Cohen's $d = 0.43$) (**Figure**
 599 **2**). In contrast, IFG→MTL ($F(1, 130) = 0.42, p > 0.05$, Cohen's $d = 0.11$), dorsal PPC→MTL
 600 ($F(1, 220) = 0.45, p > 0.05$, Cohen's $d = 0.09$), and ventral PPC→MTL ($F(1, 42) = 3.36, p > 0.05$,
 601 Cohen's $d = 0.57$) directed information flow did not differ between stimulation and non-

602 stimulation trials. We then compared the strength of top-down information flow to the MTL
 603 from the MFG, and dorsal and ventral PPC, associated with MTL stimulation. MFG→MTL
 604 directed information flow did not differ from dorsal PPC→MTL ($F(1, 28) = 0.03, p > 0.05$,
 605 Cohen's $d = 0.07$) and ventral PPC→MTL ($F(1, 137) = 0.17, p > 0.05$, Cohen's $d = 0.07$) directed
 606 information flow on stimulation trials.

607
 608 These results demonstrate that MTL stimulation reduces top-down MFG→MTL information
 609 flow in the delta-theta band during memory encoding, and that this effect is specific to PFC with
 610 no differences in either the dorsal or ventral PPC.

611
 612 *Effect of MTL stimulation on information flow from MTL to PFC and PPC during memory recall*

613
 614 We next examined the differential effects of stimulation on directed information flow from the
 615 MTL to the MFG, IFG, dPPC, and vPPC, with a 2-way ANOVA with the factors Region (MFG,
 616 IFG, dPPC, and vPPC) and Stimulation (ON/OFF) during the memory recall period which
 617 occurred ~20 sec after word encoding (**Methods**). There was no significant Stimulation x Region
 618 interaction in the delta-theta band ($F(1, 662) = 2.64, p > 0.05, \eta^2 = 3.98\text{e-}03$) (**Table 4**). However,
 619 there was a main effect of Stimulation, with higher directed information flow from the MTL to
 620 the PFC and PPC during trials with stimulation ($F(1, 662) = 7.19, p < 0.05, \eta^2 = 0.01$). There was
 621 no Stimulation x Region interaction ($F(1, 663) = 5.61, p = 0.05, \eta^2 = 8.39\text{e-}03$) or main effect of
 622 Stimulation ($F(1, 663) = 4.62, p > 0.05, \eta^2 = 6.91\text{e-}03$) in the beta-band (**Table 4**).

623
 624 *Effect of MTL stimulation on information flow to MTL from PFC and PPC during memory recall*

625

626 We next examined the differential effects of stimulation on directed information flow from the
 627 MFG, IFG, dPPC, and vPPC to the MTL, with a 2-way ANOVA with the factors Region (MFG,
 628 IFG, dPPC, and vPPC) and Stimulation (ON/OFF) during the memory recall period (**Methods**).
 629 In the delta-theta band, we found no significant Stimulation x Region interaction ($F(1, 663) =$
 630 $0.00, p > 0.05, \eta^2 = 1.49\text{e-}06$) or main effect of Stimulation ($F(1, 663) = 0.78, p > 0.05, \eta^2 =$
 631 $1.18\text{e-}03$) (**Table 4**).

632

633 We found a significant Stimulation x Region interaction for directed information flow from PFC
 634 and PPC to MTL in the beta-band ($F(1, 663) = 11.92, p < 0.01, \eta^2 = 0.02$) (**Table 4**). Post-hoc
 635 analysis of this interaction revealed that MFG→MTL directed information flow decreased during
 636 stimulation, compared to the non-stimulation, trials ($F(1, 260) = 11.11, p < 0.01$, Cohen's $d = 0.41$)
 637 (**Figure 3**). In contrast, IFG→MTL ($F(1, 130) = 3.75, p > 0.05$, Cohen's $d = 0.34$), dorsal
 638 PPC→MTL ($F(1, 220) = 1.93, p > 0.05$, Cohen's $d = 0.19$), and ventral PPC→MTL ($F(1, 41) =$
 639 $0.48, p > 0.05$, Cohen's $d = 0.22$) information flow did not differ between stimulation and non-
 640 stimulation trials. We then compared the strength of top-down information flow to the MTL from
 641 the MFG and dorsal PPC associated with MTL stimulation. This analysis revealed that
 642 MFG→MTL directed information flow was significantly lower than dorsal PPC→MTL
 643 information flow on stimulation trials ($F(1, 213) = 10.02, p < 0.01$, Cohen's $d = 0.43$) (**Figure 4**).
 644 MFG→MTL directed information flow did not differ from dorsal PPC→MTL information flow
 645 during non-stimulation trials ($F(1, 104) = 3.50, p > 0.05$, Cohen's $d = 0.37$). MFG→MTL directed
 646 information flow was lower than ventral PPC→MTL information flow during both stimulation

647 ($F(1, 149) = 17.23, p < 0.001$, Cohen's $d = 0.68$) (**Figure 4**) and non-stimulation trials ($F(1, 142)$
 648 $= 10.26, p < 0.01$, Cohen's $d = 0.56$).

649

650 Together, these results suggest that MTL stimulation reduces top-down directed information
 651 flow from the MFG subdivision of the PFC to the MTL in the beta band during memory recall.
 652 Results further suggest that MTL stimulation selectively suppresses top-down influences from
 653 the MFG, compared to both dorsal and ventral PPC, and that the PFC is relatively more sensitive
 654 to the effects of stimulation compared to the PPC.

655

656 *Effect of MTL stimulation on information flow between the MTL and the PFC and PPC in resting*
 657 *state*

658

659 To determine whether our main findings related to the direction of information flow between the
 660 MTL and the PFC and PPC in our study were specific to the effects of memory processing, we
 661 used “resting-state” data from participants collected in the UPENN-RAM public data release
 662 (Solomon et al., 2021). Subjects were instructed to sit quietly and did not perform any task.

663 Similar to the memory task, bipolar stimulation current between pairs of depth MTL electrodes
 664 was applied at 50 Hz (**Table 6**). Based on electrode placement in the MTL and the PFC and PPC
 665 brain regions and based on the criteria that the stimulation frequency was 50 Hz, we selected 2
 666 subjects ($n=105$ electrode pairs for MFG and $n=60$ electrode pairs for dPPC; IFG and vPPC did
 667 not have electrode sampling) with simultaneous electrode placements in MTL and MFG and also
 668 MTL and dPPC. We analyzed 1600 msec iEEG epochs immediately prior to the start of each
 669 stimulation trial; these correspond to the “non-stim” condition. We also analyzed 1600 msec

670 iEEG epochs immediately after the end of each stimulation trial; these correspond to the “stim”

671 condition.

672

673 We found that, in contrast to the memory task, neither MTL→MFG ($F(1, 207) = 0.04, p > 0.05$,

674 Cohen's $d = 0.03$) nor MFG→MTL ($F(1, 207) = 0.00, p > 0.05$, Cohen's $d = 0.00$) directed

675 information flow changed during stimulation, compared to the non-stimulation, trials in the delta-

676 theta frequency band. Moreover, neither MTL→MFG ($F(1, 207) = 1.44, p > 0.05$, Cohen's $d = 0.17$)

677 nor MFG→MTL ($F(1, 207) = 3.35, p > 0.05$, Cohen's $d = 0.25$) directed information flow changed

678 during stimulation, compared to the non-stimulation, trials in the beta frequency band.

679

680 Furthermore, we found that, neither MTL→dPPC nor dPPC→MTL directed information flow

681 changed during stimulation, compared to the non-stimulation, trials in both the delta-theta ($F(1, 117)$

682 $= 1.69, p > 0.05$, Cohen's $d = 0.24$ for MTL→dPPC and $F(1, 117) = 0.08, p > 0.05$, Cohen's $d = 0.05$

683 for dPPC→MTL) and beta ($F(1, 117) = 0.01, p > 0.05$, Cohen's $d = 0.02$ for MTL→dPPC and $F(1,$

684 $117) = 0.84, p > 0.05$, Cohen's $d = 0.17$ for dPPC→MTL) frequency bands.

685

686 Together, these results suggest that the reported results related to direction of information flow

687 between the MTL and the PFC and PPC that we observed during the memory task, cannot be

688 solely attributable to effects of brain stimulation causing reorganization of brain circuits, rather

689 they are related to the combined effects of stimulation and memory processing.

690

691 *Comparison of information flow between the MTL and the PFC and PPC during memory*

692 *processing and resting state*

693

694 To provide further evidence that our main findings related to the direction of information flow
 695 between the MTL and the PFC and PPC were specific to the effects of memory processing, we
 696 directly compared information flow from the MTL to the PFC and PPC, and the reverse, for the
 697 memory encoding and recall conditions with the resting-state condition, during the stimulation
 698 trials.

699
 700 We first focused our analysis on bottom-up directed information flow from the MTL to the PFC
 701 and PPC. This analysis revealed that MTL→MFG directed information flow was higher for both
 702 memory encoding ($F(1, 235) = 8.34, p < 0.01$, Cohen's $d = 0.38$) and recall ($F(1, 115) = 23.72$,
 703 $p < 0.001$, Cohen's $d = 0.91$) compared to rest, during stimulation in the delta-theta frequency
 704 band. This finding was reversed in the beta frequency band, where MTL→MFG directed
 705 information flow was lower for both memory encoding ($F(1, 233) = 16.33, p < 0.001$, Cohen's $d =$
 706 0.53) and recall ($F(1, 233) = 36.70, p < 0.001$, Cohen's $d = 0.79$) compared to rest. MTL→dPPC
 707 directed information flow was higher for both memory encoding ($F(1, 170) = 29.73, p < 0.001$,
 708 Cohen's $d = 0.83$) and recall ($F(1, 161) = 39.08, p < 0.001$, Cohen's $d = 0.99$) compared to rest,
 709 during stimulation in the delta-theta frequency band. MTL→dPPC directed information flow was
 710 also higher for memory recall ($F(1, 169) = 5.75, p < 0.05$, Cohen's $d = 0.37$) compared to rest,
 711 during stimulation in the beta band, however, MTL→dPPC directed information flow did not
 712 differ for memory encoding and rest conditions in the beta band ($F(1, 170) = 0.08, p > 0.05$,
 713 Cohen's $d = 0.04$). These results suggest that the “bottom-up” effects of stimulation on memory
 714 processing enhance MTL to PFC information flow in the delta-theta frequency band and
 715 suppress this information flow in the beta frequency band, compared to rest. On the other hand,

716 the “bottom-up” effects of stimulation on memory processing enhance MTL to PPC information
 717 flow in both delta-theta and beta frequency bands, compared to rest.

718

719 We next examined top-down directed information flow from the PFC and PPC to the MTL. This
 720 analysis revealed that MFG→MTL directed information flow was lower for both memory
 721 encoding ($F(1, 172) = 42.28, p < 0.001$, Cohen's $d = 0.99$) and recall ($F(1, 181) = 35.23, p < 0.001$,
 722 Cohen's $d = 0.88$) compared to rest, in the delta-theta frequency band and for memory recall
 723 compared to rest, in the beta frequency band ($F(1, 235) = 47.55, p < 0.001$, Cohen's $d = 0.90$).
 724 MFG→MTL directed information flow did not differ between memory encoding and rest in the
 725 beta band ($F(1, 235) = 0.05, p > 0.05$, Cohen's $d = 0.03$). dPPC→MTL directed information flow
 726 was lower for both memory encoding ($F(1, 21) = 15.00, p < 0.01$, Cohen's $d = 1.67$) and recall
 727 ($F(1, 172) = 14.26, p < 0.001$, Cohen's $d = 0.58$) compared to rest, in the delta-theta frequency
 728 band. dPPC→MTL directed information flow was higher for memory encoding ($F(1, 161) =$
 729 $15.46, p < 0.001$, Cohen's $d = 0.62$), but lower for memory recall ($F(1, 172) = 13.41, p < 0.001$,
 730 Cohen's $d = 0.56$) compared to rest, during stimulation in the beta band. These results suggest
 731 that the “top-down” effects of stimulation on memory processing mostly suppress information
 732 flow from the PFC and PPC to the MTL compared to rest.

733

734 Together, these results provide further evidence that the reported results related to direction of
 735 information flow between the MTL and the PFC and PPC, during the memory task, cannot be
 736 solely attributable to effects of brain stimulation causing reorganization of brain circuits. Rather,
 737 they are related to the combined effects of stimulation and memory processing.

738

739 *Effect of MTL stimulation on directed information flow for successful vs. unsuccessful memory*

740 *recall*

741

742 We next examine the effect of stimulation on directed information flow for successful compared
 743 to unsuccessful memory trials. To directly examine behavioral effects of stimulation, we focus
 744 our results on the memory recall periods (**Table 5**) (but see **Table 5** for results related to the
 745 memory encoding periods where strong behavioral signatures were absent). This analysis
 746 revealed that MTL→MFG directed information flow was significantly lower for successful,
 747 compared to unsuccessful, memory recall in the beta band ($F(1, 259) = 18.50, p < 0.001$, Cohen's
 748 $d = 0.53$) (**Figure 5**). MTL→vPPC directed information flow was significantly higher for
 749 successful, compared to unsuccessful, memory recall in both delta-theta ($F(1, 41) = 24.01$,
 750 $p < 0.001$, Cohen's $d = 1.62$) and beta ($F(1, 41) = 10.27, p < 0.01$, Cohen's $d = 0.77$) frequency
 751 bands (**Figure 5**).

752

753 Together, these results suggest that the strongest behavioral effects of MTL stimulation are in the
 754 bottom-up direction, mediating information flow from MTL to MFG and vPPC. Results also
 755 suggest that both stimulation and memory processing contribute to directed information flow
 756 between the MTL and the PFC and PPC that we observed during the memory task.

757

758 *Surrogate data analysis of directed information flow between the MTL and the PFC and PPC*

759

760 Next, we conducted surrogate data analysis to test the significance of the estimated PTE values
 761 compared to PTE expected by chance (**Methods**) for the stimulation trials. The estimated phases

762 from the Hilbert transform for electrodes from pairs of brain areas were time-shuffled and PTE
 763 analysis was repeated on this shuffled data to build a distribution of surrogate PTE values against
 764 which the observed PTE was tested.

765

766 Surrogate data analysis revealed that directed information flow from the MTL to MFG, IFG,
 767 dorsal PPC, and ventral PPC and in the reverse direction, were significantly higher than those
 768 expected by chance ($p < 0.05$ in all cases) in the delta-theta frequency band during both memory
 769 encoding and recall periods. In contrast, in the beta frequency band, directed information flow
 770 from the MTL to PFC and PPC subdivisions, and in the reverse direction, were significantly
 771 lower than those expected by chance ($p < 0.05$ in all cases) during both memory encoding and
 772 recall periods.

773

774 These results demonstrate that the reported directed information flow between different brain
 775 areas during stimulation trials arise from causal signaling that is enhanced significantly above
 776 chance levels.

777

778 *Effects of MTL stimulation on intra-regional information flow*

779

780 Next, we examined information flow between electrodes pairs within each of the individual brain
 781 regions examine above. We found that information flow between the electrodes did not differ
 782 between the stimulation and non-stimulation trials in any of the brain regions examined (MTL,
 783 MFG, dorsal PPC, ventral PPC) during either memory encoding or recall in the delta-theta or
 784 beta bands ($ps > 0.05$, Cohen's $d < 1.16$). However, information flow in the IFG was higher for

785 stimulation, compared to non-stimulation, trials in the beta band during memory recall ($F(1, 60)$
 786 $= 9.45$, $p < 0.05$, Cohen's $d = 0.79$). These results indicate that MTL stimulation has minimal
 787 effect on intra-regional directed information flow.

788

789 *Effects of MTL stimulation on phase synchronization between MTL and PFC and PPC*

790

791 In addition to analysis of time-delayed directed information flow using PTE, we also examined
 792 instantaneous phase synchronization between the MTL and the PFC and PPC. Analysis of
 793 instantaneous phase locking values (PLVs) (see **Methods**) revealed that phase locking of the
 794 MTL with the MFG, IFG, dorsal PPC, ventral PPC did not differ between stimulation and non-
 795 stimulation trials for either memory encoding or recall in the delta-theta or beta bands ($ps > 0.05$,
 796 Cohen's $d < 0.70$). These results suggest that the neuromodulatory effects of MTL stimulation
 797 are a consequence of the time-delayed interactions between different brain areas as precisely
 798 captured by the PTE measure rather than instantaneous synchronization measures such as the
 799 PLV.

800

801 *Effects of MTL stimulation on intra-regional phase synchronization*

802

803 Next, we used PLV to examine information flow between electrodes pairs within each of the
 804 individual brain regions. We found that phase locking between the electrodes did not differ
 805 between stimulation and non-stimulation trials in any of the brain regions during both memory
 806 encoding and recall, in the delta-theta or beta bands ($ps > 0.05$, Cohen's $d < 0.42$). These results
 807 indicate that MTL stimulation does not affect intra-region phase synchronization.

808

809 *Effects of MTL stimulation on power in each individual brain region*

810

811 We examined whether iEEG power differed between the stimulation and non-stimulation trials in
 812 each of the brain regions, as this may potentially underlie differences in directed information
 813 flow between the MTL and the PFC and PPC. We estimated power in the delta-theta and beta
 814 frequency bands (see **Methods**) for stimulation and non-stimulation trials and for both the
 815 memory encoding and recall periods. Power did not differ between stimulation and non-
 816 stimulation trials in the delta-theta or beta frequency bands in any of the brain regions ($p > 0.05$,
 817 Cohen's $d < 0.68$) (**Figure 6**).

818

819 Together, these results suggest that the differential directed information flow between the MTL
 820 and the PFC and PPC for stimulation and non-stimulation conditions are not driven by
 821 differences in the amplitude of iEEG fluctuations.

822

823 *Effects of MTL stimulation on phase-amplitude coupling*

824

825 Based on previous studies demonstrating phase-amplitude coupling (PAC) between low
 826 frequency delta-theta phase and amplitudes of high-gamma (80-160 Hz) frequency bands
 827 (Canolty et al., 2006; Tort et al., 2008), we examined the effects of stimulation on PAC in MTL,
 828 MFG, IFG, and dorsal and ventral PPC. We used the *modulation index* as an estimate of PAC in
 829 individual electrodes in different brain areas (Tort et al., 2008) (**Methods**). This analysis
 830 revealed that PAC did not differ between stimulation and non-stimulation trials in any of the

831 brain regions during memory encoding or recall ($ps>0.05$, Cohen's $d<0.80$). This suggests that
 832 stimulation of the MTL does not affect PAC in any of the five brain regions.

833 834 **Discussion**

835
836 We examined how MTL stimulation alters directed information flow between the MTL and
 837 frontoparietal cortical regions implicated in formation and monitoring of episodic memories. We
 838 used depth iEEG recordings from the UPENN-RAM cohort in which participants performed a
 839 verbal free recall task during concurrent stimulation of MTL neurons. During memory encoding,
 840 select MTL electrodes were electrically stimulated at 50 Hz on half the trials (Goyal et al., 2018;
 841 Jacobs et al., 2016). Building on our replicable prior findings of frequency specific interactions
 842 between the MTL and PFC (Das & Menon, 2021, 2022), we examined how MTL stimulation
 843 alters communication between the MTL and MFG subdivision of the PFC (i.e. dorsolateral PFC),
 844 during memory encoding, and how this stimulation altered communication during subsequent
 845 memory recall. MTL stimulation reduced memory recall (Cohen's effect size = 0.5) and
 846 disrupted directed information flow with the PFC. **Figure 7** summarizes our key findings.

847
848 MTL stimulation decreased MFG→MTL information flow in the delta-theta frequency band
 849 during the encoding period. Furthermore, the effects of MTL stimulation carried over from the
 850 encoding to the subsequent memory recall period, despite a ~20 sec delay period in which there
 851 was no external stimulation of the MTL. This process was characterized by decreased top-down
 852 MFG→MTL information flow in the beta frequency band. However, there was no difference in
 853 top-down PPC→MTL information flow. A direct comparison between the PFC and PPC
 854 revealed stronger modulation of top-down influences on the MTL from the PFC, compared to the
 855 PPC. Together, these findings demonstrate that MTL stimulation disrupts processing specifically

856 in the PFC in the low frequency delta-theta range during memory encoding with aftereffects that
857 extend to subsequent recall periods.

858

859 *MTL stimulation effects on directed MTL → PFC and PFC → MTL information flow during*
860 *memory encoding*

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862 The primary goal of our study was to characterize the effect of MTL stimulation on directed
863 information flow between the MTL and the PFC during verbal episodic memory processing. The
864 MTL and MFG (dorsolateral PFC) play a critical role in human episodic memory encoding
865 (Anderson et al., 2010; Ekstrom & Watrous, 2014; Gonzalez et al., 2015; Neuner et al., 2014;
866 Watrous et al., 2013). However, it is unclear how electrical stimulation of the MTL modulates
867 neural dynamics of the targeted regions and the circuits that link them. Specifically, the effect of
868 stimulation on directed information flow between the MTL and the PFC during episodic memory
869 processing is poorly understood.

870

871 Our study builds on previously replicated findings across verbal episodic and spatial memory
872 domains which revealed higher bottom-up MTL → PFC information flow than the reverse, in
873 delta-theta and higher top-down PFC → MTL information flow than the reverse, in the beta
874 frequency bands (Das & Menon, 2021, 2022). We used phase transfer entropy (PTE), which
875 provides a robust and powerful tool for characterizing information flow between brain regions
876 based on phase coupling (Hillebrand et al., 2016; Lobier et al., 2014; M. Y. Wang et al., 2017).
877 We took an unbiased approach for assigning electrodes to individual anatomically-defined brain
878 regions and we did not select electrodes based on arbitrary task or stimulation-induced activation

879 profiles. Our approach thus allowed us to probe the electrophysiological correlates of the effects
880 of MTL stimulation on directed information flow between the MTL and PFC more generally.
881 We found that MTL stimulation decreased PFC→MTL information flow during the encoding
882 period, in delta-theta band. Notably, these effects were specific to the dorsolateral MFG
883 subdivision of the PFC and were not observed in the more ventral aspects that comprise the IFG.

884
885 We conducted control analyses to ensure that the reported effects related to the directed
886 information flow between the MTL and the MFG did not arise solely from brain stimulation
887 causing reorganization of brain circuits. Specifically, we used “resting-state” data from a
888 separate group of participants, also acquired and released as part of the UPENN-RAM public
889 data release (Solomon et al., 2021). Participants were instructed to sit quietly and did not perform
890 any task. Similar to the memory task, in the resting-state condition, bipolar stimulation current
891 between pairs of depth MTL electrodes was applied at 50 Hz. We found that, in contrast to the
892 memory task, neither MTL→MFG nor MFG→MTL directed information flow changed during
893 stimulation, compared to the non-stimulation, trials in the delta-theta frequency band. These
894 results suggest that directed information flow between the MTL and the MFG observed during
895 the memory task are not solely attributable to brain stimulation-induced reorganization of brain
896 circuits, rather they are related to the combined effects of stimulation and memory processing.

897
898 *MTL stimulation effects on directed MTL →PFC and PFC→MTL information flow during*
899 *memory recall*

900

901 Crucially, the effects of MTL stimulation were also detectable in the subsequent recall period
 902 which occurred after a delay of 20 seconds. This finding is consistent with previous human iEEG
 903 studies which have observed strong afterdischarge iEEG signals within and outside the MTL
 904 during memory retrieval, which occurred tens of seconds after MTL stimulation was applied
 905 during the encoding period of an episodic memory task (Halgren et al., 1985; Jun et al., 2020).
 906 Moreover, similar to our findings, these afterdischarge effects were linked to memory
 907 impairment in these studies (Halgren et al., 1985; Jun et al., 2020). Specifically, we observed
 908 decreased MFG→MTL information flow on stimulation, compared to non-stimulation, trials in
 909 the beta frequency band. Again, this effect was specific to the dorsolateral MFG subdivision of
 910 the PFC, which is known to play a prominent role in top-down control of both subcortical and
 911 cortical regions involved in memory formation (Brovelli et al., 2004; Engel & Fries, 2010;
 912 Spitzer & Haegens, 2017; Stanley, Roy, Aoi, Kopell, & Miller, 2018). Extending our findings of
 913 spectrally resolved top-down influences from the PFC, we found MTL stimulation effects in the
 914 beta-band but not in the delta-theta frequency band, providing consistent evidence for spectral
 915 dissociation associated with the beta frequency band. Theoretical models have pointed to both
 916 excitatory and inhibitory mechanisms underlying deep brain stimulation (McIntyre, Grill,
 917 Sherman, & Thakor, 2004; Vitek, 2002). We did not observe changes in power of iEEG signals
 918 in either frequency band, suggesting causal circuit mechanisms arising from phase, rather than
 919 amplitude, changes underlie the observed MTL stimulation related changes in information flow.
 920
 921 LFP studies in monkeys have demonstrated a more prominent role for the dorsal, compared to
 922 the ventral PFC, in top-down control in the beta frequency band for processing higher level
 923 abstractions during working memory performance (Wutz, Loonis, Roy, Donoghue, & Miller,

2018). Electrophysiology studies in rodents performing an odor-place associative memory guided decision task on a T-maze have shown that hippocampal-PFC coherence in the beta frequency band is linked to accurate decisions (Symanski, Bladon, Kullberg, Miller, & Jadhav, 2022). LFP studies in monkeys performing a paired association learning task have shown that beta oscillations in the MFG encode picture-color association (Tanigawa et al., 2022). fMRI studies in humans have shown that the dorsal MFG is a part of the central executive network which plays an important role in memory processing and complex decision making (Menon & Uddin, 2010; Seeley et al., 2007; Sridharan, Levitin, & Menon, 2008). Additionally, magnetoencephalography and iEEG studies in humans have shown a prominent role of beta for feedback signaling (Hayat et al., 2022; Michalareas et al., 2016). Consistent with our findings, rodent studies have also shown that inhibition of PFC projections to the hippocampus impairs memory recall (Rajasethupathy et al., 2015; Yadav et al., 2022). Reduction in neural signaling from the MFG to the MTL during memory recall may explain why stimulation of the MTL reduces or impairs memory performance (Coleshill et al., 2004; Goyal et al., 2018; Jacobs et al., 2016; Lacruz et al., 2010).

A recent study using 1 Hz repetitive transcranial magnetic stimulation (rTMS) of the MFG found enhancement of verbal memory performance and also showed that this stimulation induced stronger beta power modulation in the posterior areas (van der Plas et al., 2021), suggesting that neuromodulatory effects in the MFG might be the most prominent in the beta frequency band. A meta-analysis of rTMS studies has revealed that 1 Hz rTMS of the MFG usually leads to an enhancement of episodic memory performance, whereas 20 Hz rTMS of the MFG usually leads to a reduction in episodic memory performance (Yeh & Rose, 2019). These results indicate a

947 disruptive effect of beta on MFG neural dynamics at frequencies significantly greater than 1 Hz,
 948 including the 50 Hz stimulation frequency used in our study, and may explain the reduction of
 949 information flow from the MFG that we observed during the recall periods in this frequency
 950 band.

951

952 *Dissociable effects of MTL stimulation on top-down causal information flow from PFC and PPC*

953

954 The next goal of our study was to contrast the effects of MTL stimulation on information flow
 955 with the PFC and PPC. In addition to the PFC, the PPC also plays an important role in episodic
 956 memory (C. Moscovitch, Kapur, Köhler, & Houle, 1995; Schacter, Alpert, Savage, Rauch, &
 957 Albert, 1996; Tulving et al., 1994). PTE analysis revealed that, in contrast to the PFC, there were
 958 no differences between stimulation and non-stimulation trials in top-down dorsal PPC→MTL
 959 information flow. A direct comparison revealed stronger MTL stimulation-induced modulation
 960 of top-down MFG→MTL, compared to dorsal PPC→MTL in the beta frequency band (**Figure**
 961 **4**). Information flow between the MTL and ventral PPC was unaffected by MTL stimulation, and
 962 a direct comparison confirmed stronger MTL stimulation-induced modulation of top-down
 963 MFG→MTL, compared to ventral PPC→MTL in the beta frequency band. This suggests that the
 964 dorsolateral MFG subdivision of the PFC is more sensitive to MTL stimulation than PPC regions
 965 involved in episodic memory.

966

967 Electrophysiology studies in monkeys have shown that the PFC is more sensitive to memory
 968 encoding compared to the PPC (Dang, Li, Pu, Qi, & Constantinidis, 2022; Masse, Hodnefield, &
 969 Freedman, 2017; Murray, Jaramillo, & Wang, 2017; Qi, Elworthy, Lambert, & Constantinidis,

2015; Zhou et al., 2021). Specifically, these studies showed that, compared to the PPC, neurons in the PFC are more responsive (Dang et al., 2022), show more persistent firing rate (Masse et al., 2017), and are more robust to distractors (Murray et al., 2017; Qi et al., 2015; Zhou et al., 2021). Together, these findings suggest that the MFG may play an enhanced role compared to the PPC in memory formation, which may make it a more sensitive target of brain stimulation compared to the PPC in humans (J. X. Wang et al., 2014).

Behavioral specificity of the effects of MTL stimulation

Finally, we examined whether the observed effects of MTL stimulation on information flow between different brain regions reflect cognitive processes related to memory encoding, or whether they are solely attributable to the reorganization of brain circuits from the effects of stimulation. We tested the hypothesis that the information flow between different brain areas would differ between successful and unsuccessful memory trials during stimulation, thus putatively reflecting cognitive processes related to memory processing, rather than effects of stimulation only.

We found that the direction of information flow between the MTL and both the PFC and PPC during memory recall is behaviorally relevant. Results support the hypotheses that causal signaling from the MTL to both regions are associated with memory recall processes, rather than arising solely from the effects of MTL stimulation-related reorganization of brain circuits. MTL→MFG directed information flow was significantly lower for successful, compared to

992 unsuccessful, memory recall in the beta band. This suggests that the higher causal signaling
 993 between the MTL→MFG in the beta band during unsuccessful trials is disruptive during recall.
 994
 995 Crucially, we found that the direction of information flow between the MTL and the ventral PPC
 996 during memory recall was also behaviorally relevant. MTL→vPPC directed information flow
 997 was significantly higher for successful, compared to unsuccessful, memory recall in both the
 998 delta-theta and beta frequency bands. MTL-vPPC have been previously proposed to form a
 999 coherent set of network and interactions within this network have been proposed to play a crucial
 1000 role in memory processing in humans (Ranganath & Ritchey, 2012; Wagner et al., 2005).
 1001 Moreover, non-invasive rTMS to the vPPC area is known to be associated with successful
 1002 associative memory retrieval in humans (J. X. Wang et al., 2014). The increased MTL→vPPC
 1003 directed information flow that we observed for the successful trials during memory recall is thus
 1004 consistent with the prominent role of the vPPC for episodic memory retrieval and extends our
 1005 understanding of directed causal signaling that supports such a role in the human brain.
 1006
 1007 Together, these results demonstrate that stimulating the MTL has a significant impact on
 1008 communication between the MTL and the PFC and PPC, which can either enhance or hinder
 1009 memory recall. Additionally, the results indicate that the direction of information flow in the
 1010 MTL is not solely due to reorganization of brain circuits caused by stimulation, but rather a
 1011 combination of stimulation and memory processing

1013 *Limitations*

1014

1015 The stimulation paradigm used in the study was applied only at a single frequency (50 Hz)
 1016 **(Methods)**. Previous studies in humans have usually applied direct stimulation at theta and
 1017 gamma frequencies to modulate memory performance, which are considered to be the
 1018 endogenous rhythms of the MTL (Eichenbaum, 2017), although these frequencies have had a
 1019 varied effect on memory performance. Whereas theta frequency stimulation have shown
 1020 improvement in memory performance (Alagapan et al., 2019; Koubesssi, Kahriman, Syed,
 1021 Miller, & Durand, 2013; Lee et al., 2013), stimulation at 50 Hz has shown heterogeneous
 1022 patterns of memory performance, with some studies suggesting memory enhancement (Fell et
 1023 al., 2013; Inman et al., 2018; Suthana et al., 2012), while others have found impairment in
 1024 memory performance (Coleshill et al., 2004; Goyal et al., 2018; Jacobs et al., 2016; Lacruz et al.,
 1025 2010). Limitations of electrode placement precluded analysis of causal circuit dynamics
 1026 associated with each hemisphere and distinct subdivisions of the MTL; denser sampling of
 1027 electrodes in multiple brain regions with a wider range of experimental tasks, and a larger
 1028 number of participants are needed to further address these limitations. Additionally, studies with
 1029 memory and resting-state iEEG data acquired in the same participants are needed to confirm that
 1030 the effects of MTL stimulation reported in our study are not solely attributable to brain
 1031 stimulation-induced reorganization of brain circuits. Finally, it is not known whether some of the
 1032 patients may have shown considerable memory dysfunction in formal neuropsychological
 1033 testing. Future studies with rigorous neuropsychological testing procedures are needed to
 1034 determine the effect of brain stimulation in patients with different cognitive abilities.
 1035
 1036 In the present study, participants received stimulation at a range of current amplitudes, starting
 1037 from 0.25 mA to 1.5 mA. The choice of the current amplitude values for the cognitive

1038 experiments of the participants was the maximum current for each site that could be applied
1039 without inducing patient symptoms, epileptiform after discharges, or seizures. Lack of sufficient
1040 participants and electrode pairs for each of these current amplitude values did not allow us to
1041 study the effects of current amplitude on the information flow between the MTL and the PFC
1042 and PPC. Future studies will also need to consider the effects of a range of stimulation
1043 frequencies and currents, and electrode sites across MTL subdivisions in gray/white matter to
1044 rigorously assess other factors that influence memory performance, monitoring and directed
1045 information flow between the MTL and PFC.

1046

1047 *Conclusions*

1048

1049 Our findings provide novel evidence that MTL stimulation alters directed information flow with
1050 the PFC and PPC and that these influences are behaviorally relevant. Stimulating the MTL
1051 decreased flow of information from PFC to the MTL during both the encoding and recall
1052 periods, with effects lasting for more than 20 seconds after end of stimulation. This suppression
1053 of top-down PFC to MTL influences was stronger than suppression of PPC to MTL influences.
1054 Additionally, the flow of information from MTL to PFC was lower during successful memory
1055 recall compared to unsuccessful recall, while the flow of information from the MTL to the
1056 ventral PPC was higher during successful recall. These results show that the effects of MTL
1057 stimulation are specific to behavior, region, and direction, that MTL stimulation specifically
1058 impairs communication with the PFC, and that causal MTL-ventral PPC circuits support
1059 successful memory recall. Findings further suggest that information theoretic measures based on
1060 phase delays may provide a more robust measure of the effects of stimulation than other

1061 measures such as changes in power and phase-amplitude coupling. Crucially, our findings
1062 demonstrate that suppression of the dorsolateral PFC is a locus of circuit vulnerability induced
1063 by MTL stimulation. Findings uncover a mechanism by which human MTL stimulation disrupts
1064 both formation and retrieval of recent memories (Halgren et al., 1985). Our findings have
1065 implications for translational applications aimed at realizing the promise of brain stimulation-
1066 based treatment of memory disorders.

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Figure captions

Figure 1. (a) Intracranial stimulation sites in the medial temporal lobe (MTL) investigated in this study. Each anode-cathode pair of electrodes is connected by a red line. MTL included the hippocampus, parahippocampal gyrus, and entorhinal cortex. **(b) Non-stimulation iEEG recording sites in the MTL, middle and inferior frontal gyrus subdivisions of the prefrontal cortex (MFG and IFG), and dorsal and ventral subdivisions of the posterior parietal cortex (dPPC and vPPC), investigated in this study. (c) Event structure of the verbal episodic memory task during non-stimulation (top panel) and stimulation (bottom panel) trials used in this study** (see **Methods** for details). Participants were first presented with a list of words in the encoding block and asked to recall as many as possible from the original list after a short delay (distractor period). Stimulation was provided in a blocked pattern; the stimulator was active during the presentation of a pair of consecutive words and then inactive for the following pair. On each stimulated list, the stimulator was active for half the total words (see **Methods** for details).

Figure 2. Directed information flow from PFC and PPC to the MTL in delta-theta band (0.5-8 Hz) during stimulation, compared to non-stimulation, trials in the memory encoding period. MFG → MTL information flow, measured using phase transfer entropy (PTE), was reduced during the stimulation, compared to non-stimulation, trials (n=132). In contrast, IFG→MTL (n=68), dorsal PPC→MTL (n=114), and ventral PPC→MTL (n=23) directed information flow did not differ between stimulation and non-stimulation trials. The central mark indicates the median, and the bottom and top edges of the box indicate the 25th and 75th percentiles, respectively. Whiskers extend to the most extreme data points not considered outliers. dPPC = dorsal PPC, vPPC = ventral PPC. ** $p < 0.01$ (FDR-corrected).

Figure 3. Directed information flow from the PFC and PPC to the MTL in beta band (12-30 Hz) during stimulation, compared to non-stimulation, trials in the memory recall period. MFG → MTL information flow was reduced during the stimulation trials compared to the non-stimulation trials (n=132). In contrast, IFG→MTL (n=68), dorsal PPC→MTL (n=114), and ventral PPC→MTL (n=23) directed information flow did not differ between stimulation and non-stimulation trials. dPPC = dorsal PPC, vPPC = ventral PPC. ** $p < 0.01$ (FDR-corrected).

Figure 4. Comparison of directed information flow from the MFG and dorsal/ventral PPC to the MTL in beta band (12-30 Hz) during stimulation trials in the memory recall period. MFG → MTL (n=132) information flow was significantly lower during the stimulation trials compared to both dorsal PPC→MTL (n=114) and ventral PPC→MTL (n=23) information flow. dPPC = dorsal PPC, vPPC = ventral PPC. *** $p < 0.001$, ** $p < 0.01$ (FDR-corrected).

Figure 5. Comparison of directed information flow from the MTL to the MFG and vPPC for successful compared to unsuccessful recall, during stimulation trials in the memory recall period. MTL → MFG (n=132) information flow was significantly reduced during successful, compared to unsuccessful, recall in the beta band. Moreover, MTL→ventral PPC (n=23) information flow was significantly higher during successful, compared to unsuccessful, recall in both the delta-theta and beta frequency bands. *** $p < 0.001$, ** $p < 0.01$ (FDR-corrected).

Figure 6. Spectral power in the delta-theta (0.5-8 Hz) and beta (12-30 Hz) frequency bands during stimulation compared to non-stimulation trials for the encoding and retrieval periods. (a) Spectral power in the delta-theta band during encoding periods. **(b)** Spectral power in the delta-theta band during recall periods. **(c)** Spectral power in the beta band during encoding periods. **(d)** Spectral power in the beta band during recall periods. Zero on the x-axis denotes the onset of word presentation for the encoding periods and the verbal recall of a word during the recall periods.

Figure 7. Schematic illustration of key findings related to MTL stimulation. (a) Directed information flow on successful trials. MTL stimulation decreased concurrent directed information flow from the middle frontal gyrus (MFG) subdivision of the prefrontal cortex to the MTL during memory encoding (delta-theta band). These effects were specific to MFG and were not observed in inferior frontal gyrus (IFG) or dorsal or ventral nodes of posterior parietal cortex. MTL stimulation aftereffects were observed in the subsequent memory recall period more than 20 seconds later, characterized by decreased top-down information flow from MFG to MTL (beta band); again, these effects were specific to MFG and were not observed in IFG or dorsal or ventral nodes of the posterior parietal cortex. Blue arrows show decrease during stimulation, compared to non-stimulation trials. **(b) Comparison of directed information flow during successful vs. unsuccessful memory recall.** MTL to MFG information flow on stimulation trials was significantly lower for successful, compared to unsuccessful, memory recall (beta band). In contrast, MTL to ventral posterior parietal cortex (PPC) information flow was significantly higher for successful, compared to unsuccessful, memory recall (both delta-theta and beta bands). Thickness of arrows correspond to relative strength of information flow, with higher thickness denoting stronger information flow.

Tables

Table 1. Participant demographic information for the memory task and stimulation details (total 14 participants).

Participant ID	Gender	Age	Stimulation electrode type (D= "depth")	Stimulation current amplitude
001	F	48	D	1 mA
003	F	39	D	1.5 mA
020	F	48	D	1.5 mA
030	M	23	D	1 mA
031	M	40	D	1.5 mA
033	F	31	D	1 mA
035	F	45	D	0.5 mA
056	M	34	D	1.5 mA
077	F	47	D	1 mA
085	F	30	D	1.5 mA
101	F	26	D	0.5 mA
111	M	20	D	0.75 mA
112	F	29	D	0.5 mA
150	F	49	D	0.25 mA

Table 2. Number of electrode pairs used in the phase transfer entropy (PTE) and phase locking value (PLV) analysis. MTL: medial temporal lobe; MFG: middle frontal gyrus, IFG: inferior frontal gyrus, dPPC: dorsal posterior parietal cortex; vPPC: ventral posterior parietal cortex.

Network pairs	Number of electrode pairs (n)	Number of participants	Participant IDs (Gender/Age)
MTL-MFG	132	4	003 (F/39), 020 (F/48), 033 (F/31), 077 (F/47)
MTL-IFG	68	5	003 (F/39), 020 (F/48), 035 (F/45), 077 (F/47), 101 (F/26)
MTL-dPPC	114	8	001 (F/48), 003 (F/39), 020 (F/48), 033 (F/31), 035 (F/45), 077 (F/47), 101 (F/26), 111 (M/20)
MTL-vPPC	23	4	033 (F/31), 077 (F/47), 101 (F/26), 111 (M/20)

Table 3. Number of electrodes in each brain region, used in power and phase-amplitude coupling analysis. MTL: medial temporal lobe; MFG: middle frontal gyrus, IFG: inferior frontal gyrus, dPPC: dorsal posterior parietal cortex; vPPC: ventral posterior parietal cortex.

Brain regions	Number of electrodes (n)	Number of participants	Participant IDs (Gender/Age)
MTL	30	10	001 (F/48), 003 (F/39), 020 (F/48), 031 (M/40), 033 (F/31), 035 (F/45), 077 (F/47), 101 (F/26), 111 (M/20), 112 (F/29)
MFG	51	7	003 (F/39), 020 (F/48), 030 (M/23), 033 (F/31), 056 (M/34), 077 (F/47), 085 (F/30)
IFG	35	9	003 (F/39), 020 (F/48), 030 (M/23), 035 (F/45), 056 (M/34), 077 (F/47), 085 (F/30), 101 (F/26), 150 (F/49)
dPPC	52	11	001 (F/48), 003 (F/39), 020 (F/48), 030 (M/23), 033 (F/31), 035 (F/45), 056 (M/34), 077 (F/47), 085 (F/30), 101 (F/26), 111 (M/20)
vPPC	9	4	033 (F/31), 077 (F/47), 101 (F/26), 111 (M/20)

1672 **Table 4. Differential effects of stimulation on directed information flow between the MTL**
 1673 **and the MFG, IFG, dPPC, and vPPC. Results from 2-way ANOVA analysis with factors**
 1674 **Region (MFG, IFG, dPPC, and vPPC) and Stimulation (ON/OFF).** Statistically significant *p*-
 1675 values of interaction, and main effects of Stimulation when interactions were non-significant, are
 1676 indicated in bold (FDR-corrected for multiple comparisons).
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Direction	Interaction effect (0.5-8 Hz)	Interaction effect (12-30 Hz)	Stimulation main effect (0.5-8 Hz)	Stimulation main effect (12-30 Hz)
Encode (MTL→PFC, PPC)	0.9138971	0.5496000	0.07382400	0.79940000
Encode (PFC, PPC→MTL)	0.0025908	0.5496000	0.00146600	0.41133333
Recall (MTL→PFC, PPC)	0.2090900	0.0482400	0.02006667	0.05436000
Recall (PFC, PPC→MTL)	0.9749598	0.0025908	0.42993429	0.00076512

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Table 5. Differential effects of MTL stimulation on directed information flow for successful vs. unsuccessful memory during (a) Encoding and (b) Recall periods. Statistically significant *p*-values are indicated in bold (FDR-corrected for multiple comparisons).

(a) Memory Encoding

Direction	0.5-8 Hz	12-30 Hz
MTL→MFG	0.0252080	0.9950
MTL→IFG	0.9338286	0.9950
MTL→dPPC	0.0252080	0.9950
MTL→vPPC	0.9338286	0.9950

MFG→MTL	0.9338286	0.8712
IFG→MTL	0.9958000	0.9950
dPPC→MTL	0.9338286	0.9950
vPPC→MTL	0.9338286	0.9950

(b) Memory Recall

Direction	0.5-8 Hz	12-30 Hz
MTL→MFG	0.29573333	0.00017304
MTL→IFG	0.09964000	0.50540000
MTL→dPPC	0.44040000	0.04010667
MTL→vPPC	0.00012136	0.00869200

MFG→MTL	0.50053333	0.32848000
IFG→MTL	0.50053333	0.39906667
dPPC→MTL	0.68120000	0.32848000
vPPC→MTL	0.68120000	0.50540000

1734 **Table 6. Participant demographic information for analysis of resting-state iEEG (total 2**
1735 **participants).**

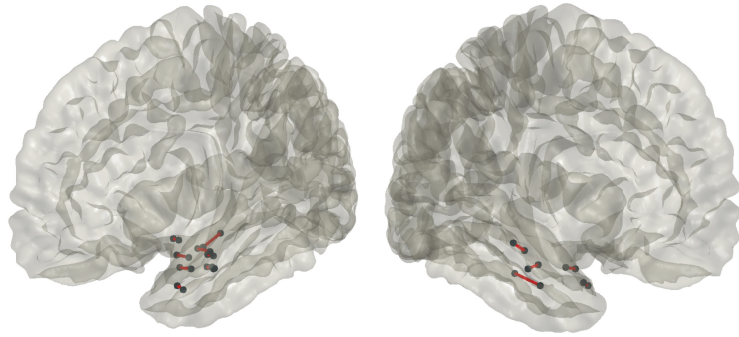
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Participant ID	Gender	Age	Stimulation electrode type (D= “depth”)	Stimulation current amplitude	Stimulation duration
054	M	23	D	1 mA	250 ms
136	F	56	D	2 mA	500 ms

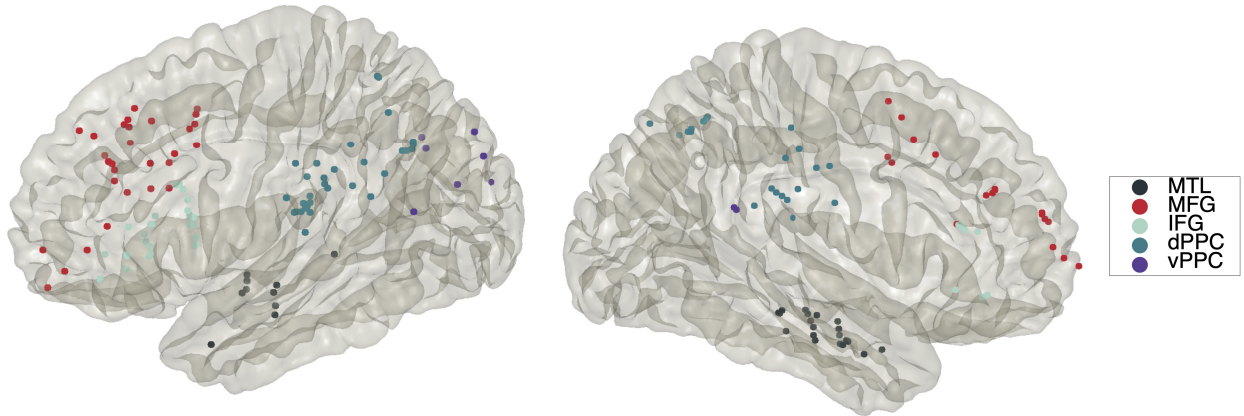
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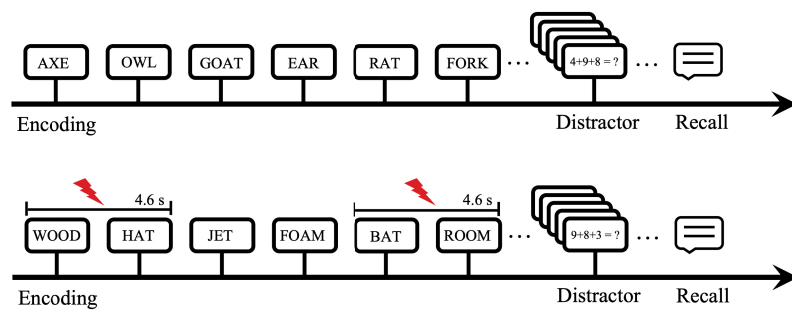
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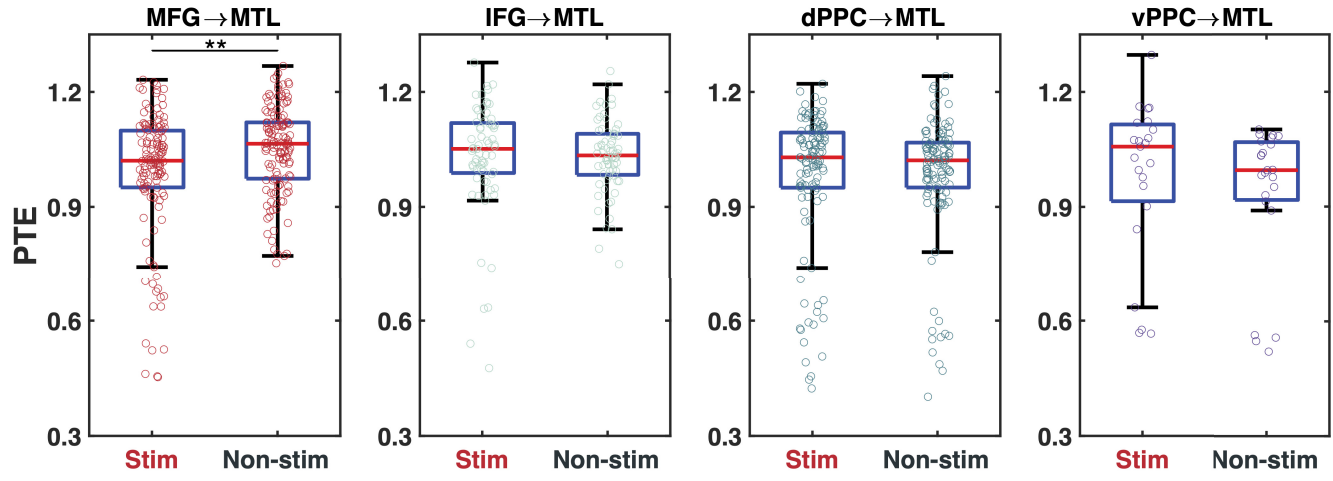


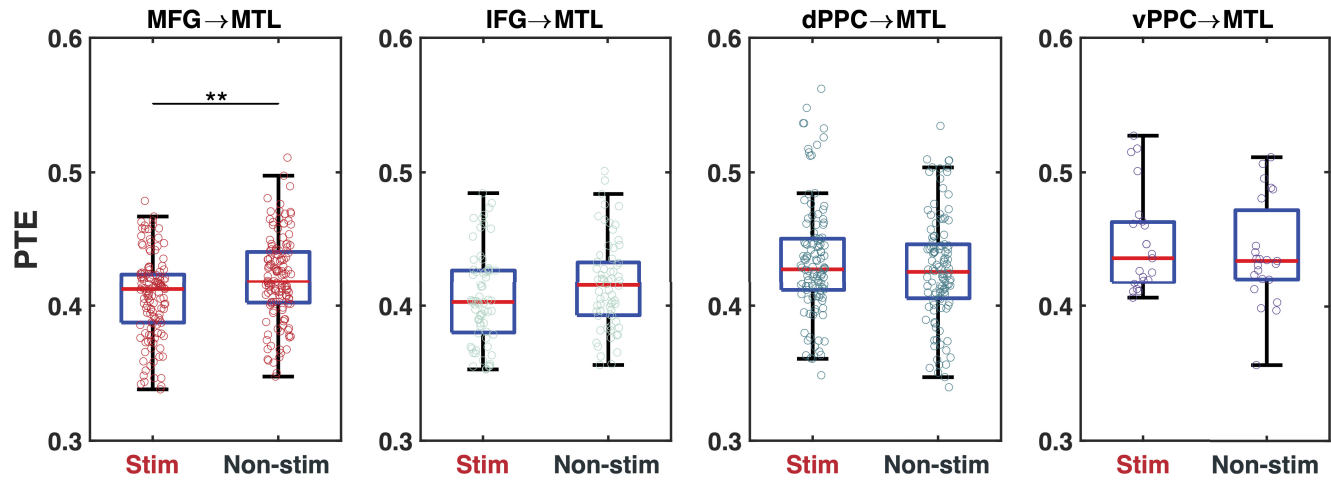
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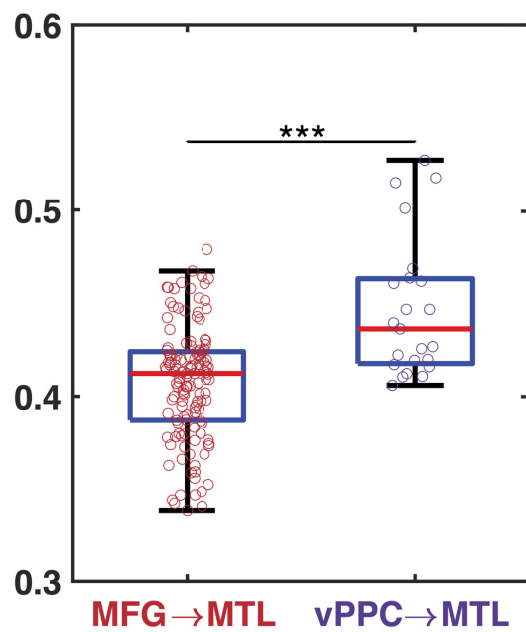
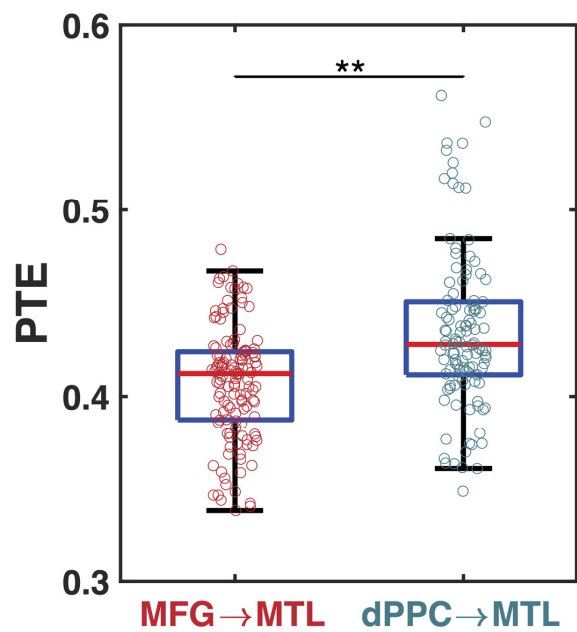


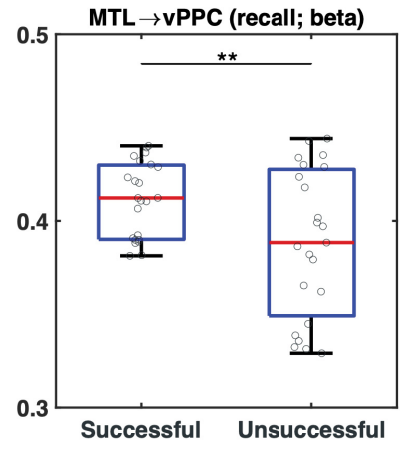
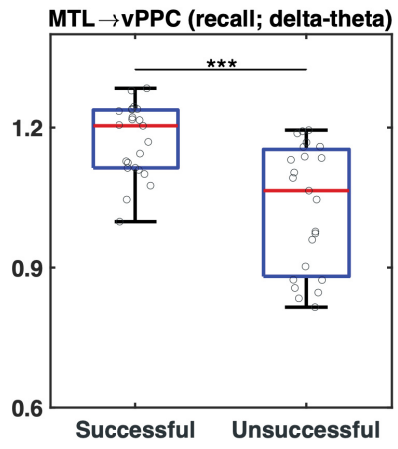
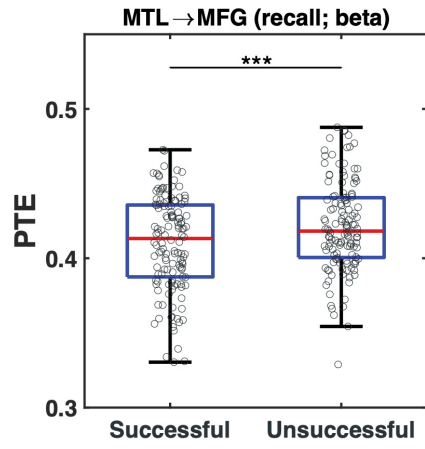
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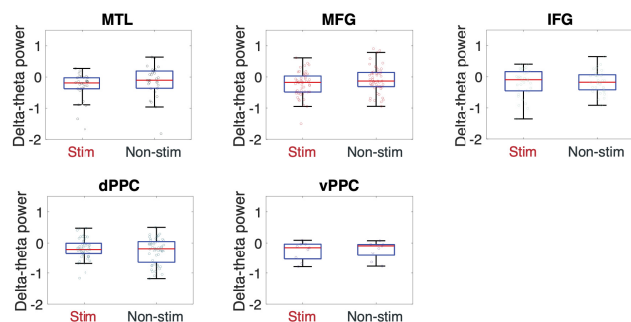
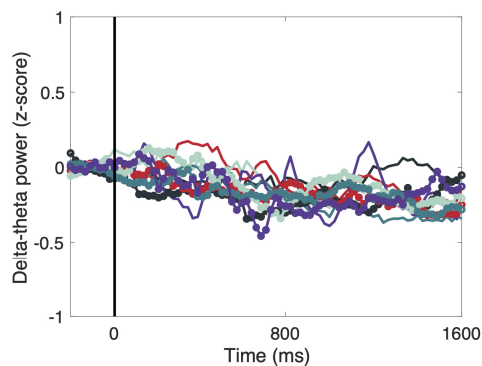




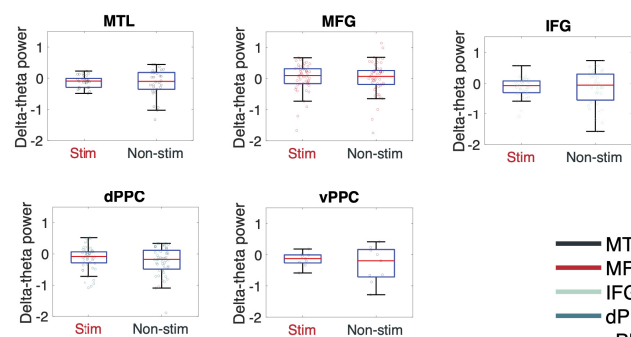
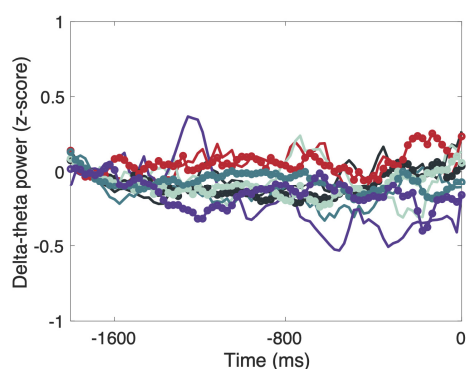




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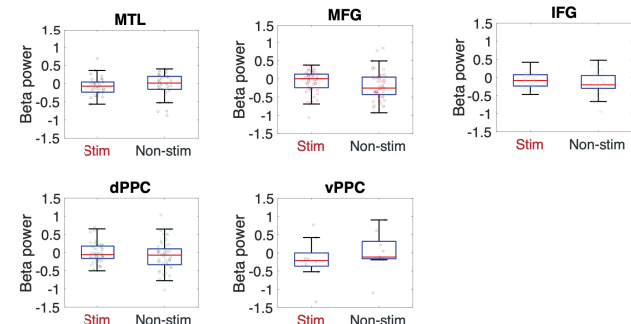
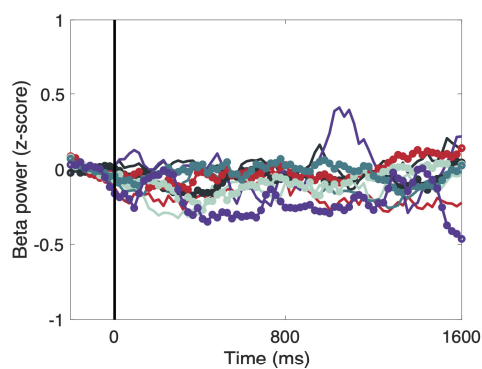


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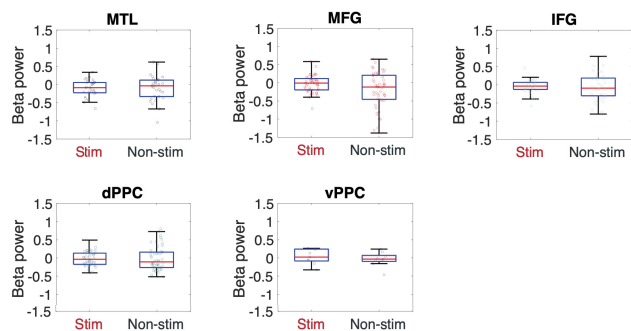
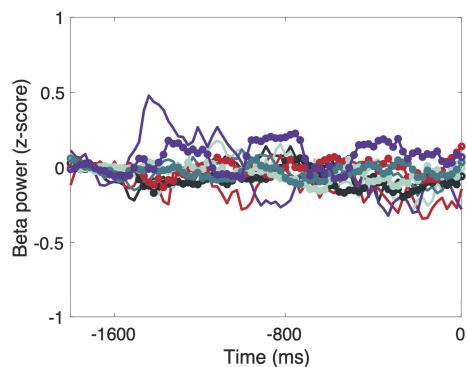


— MTL
— MFG
— IFG
— dPPC
— vPPC
● Stim
— Non-stim

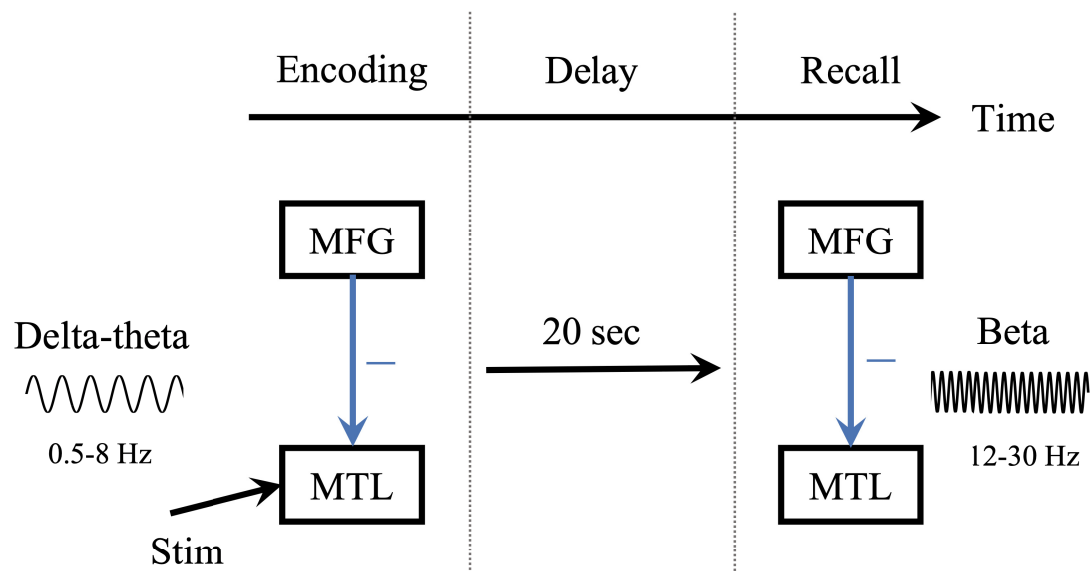
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